



# Dosimetry Needs and Methods for SRT: Lu-177

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NCI Workshop on Dosimetry of Systemic Radiopharmaceutical Therapy (SRT) Rockville, MD, April 19-20, 2018

# Disclosures

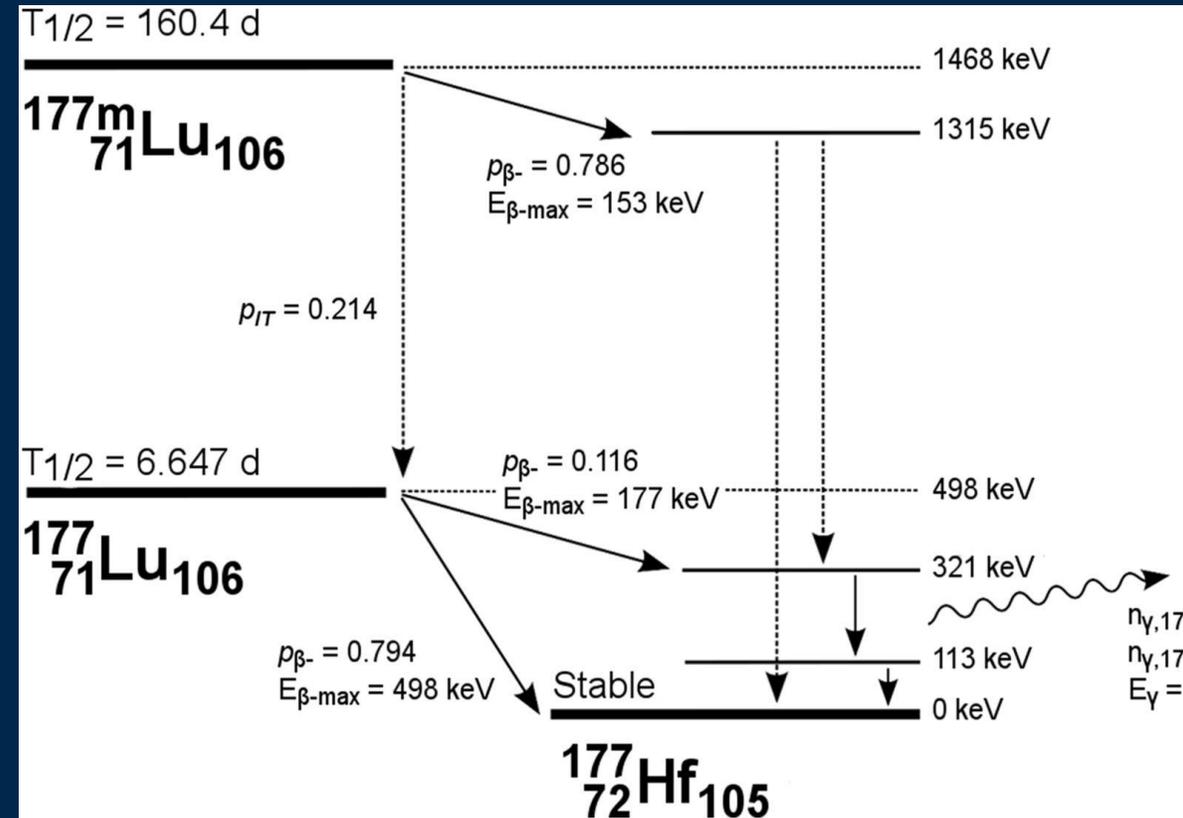
- Yuni Dewaraja is a consultant for MIM Software, Inc.

# Lu-177 Imaging/Dosimetry

- Used in targeted radionuclide therapies
  - PRRT for NETs (Lu-177 DOTATATE)
  - Lu-177 PSMA for metastatic prostate cancer
  - RIT for NHL (177Lu-Lilotomab Satetraxetan)
- $\beta$ -emitter:  $E_{\text{ave}}=147$  keV;  $E_{\text{max}}=498$  keV; mean tissue penetration=0.7 mm, max = 1.5 mm;  $T_{1/2}=6.7$  d
  - More suitable for irradiating small tumor with less damage to normal tissue compared with Y-90
  - Gamma-ray emissions suitable for single-photon imaging

# Decay Scheme

- Two low intensity  $\gamma$  rays
  - 208.4 (10.36%), 112.9 keV(6.17%)
    - Typically not used for pre-therapy tracer imaging
- Produced by neutron activation by  $^{176}\text{Lu}(n,\gamma)^{177}\text{Lu}$  reaction.
  - Long lived isomer  $^{177\text{m}}\text{Lu} < 0.05\%$  at a reference time of production



# Quantitative Lu-177 SPECT/CT for Dosimetry

## MIRD Pamphlet No. 26: Joint EANM/MIRD Guidelines for Quantitative $^{177}\text{Lu}$ SPECT Applied for Dosimetry of Radiopharmaceutical Therapy

Michael Ljungberg<sup>1</sup>, Anna Celler<sup>2</sup>, Mark W. Konijnenberg<sup>3</sup>, Keith F. Eckerman<sup>4</sup>, Yuni K. Dewaraja<sup>5</sup>, and Katarina Sjögren-Gleisner<sup>1</sup>

In collaboration with the SNMMI MIRD Committee: Wesley E. Bolch, A. Bertrand Brill, Frederic Fahey, Darrell R. Fisher, Robert Hobbs, Roger W. Howell, Ruby F. Meredith, George Sgouros, and Pat Zanzonico, and the EANM Dosimetry Committee: Klaus Bacher, Carlo Chiesa, Glenn Flux, Michael Lassmann, Lidia Strigari, and Stephan Walrand.

<sup>1</sup>Department of Medical Radiation Physics, Lund University, Lund, Sweden; <sup>2</sup>Radiology Department, Medical Imaging Research Group, University of British Columbia, Vancouver, Canada; <sup>3</sup>Department of Nuclear Medicine, Erasmus University Medical Center, Rotterdam, Holland; <sup>4</sup>Easterly Scientific, Knoxville, Tennessee; and <sup>5</sup>Department of Radiology, University of Michigan Medical School, Ann Arbor, Michigan

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The accuracy of absorbed dose calculations in personalized internal radionuclide therapy is directly related to the accuracy of the activity (or activity concentration) estimates obtained at each of the imaging time points. MIRD Pamphlet no. 23 presented a general overview of methods that are required for quantitative SPECT imaging. The present document is next in a series of isotope-specific guidelines and recommendations that follow the general information that was provided in MIRD 23. This paper focuses on  $^{177}\text{Lu}$  (lutetium) and its application in radiopharmaceutical therapy.

**Key Words:** image processing; oncology; endocrine; radiobiology/dosimetry; radionuclide therapy; SPECT/CT; guideline; lutetium; quantitative SPECT

**J Nucl Med 2016; 57:151–162**

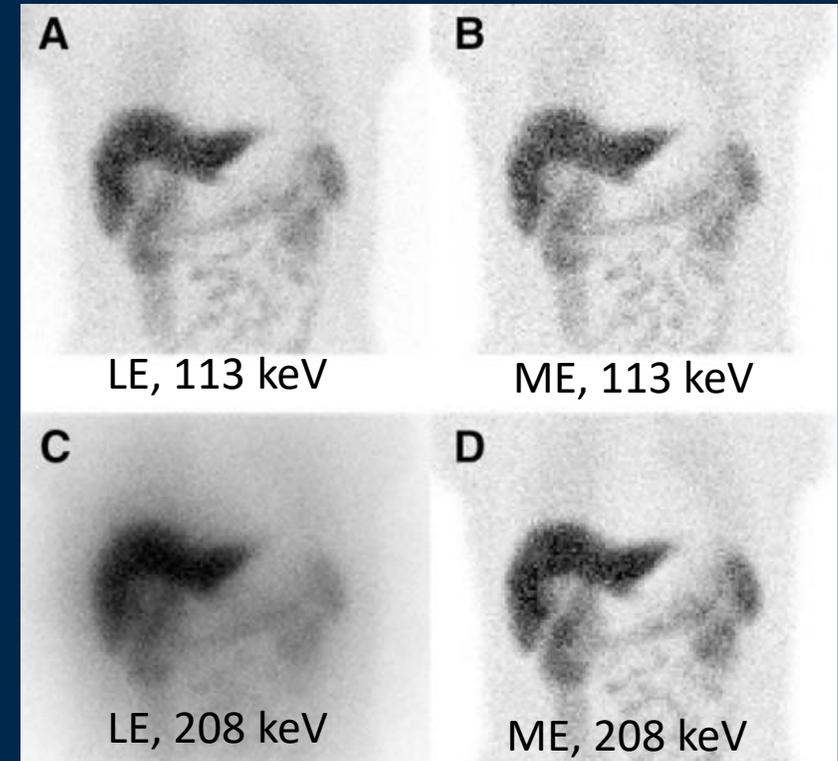
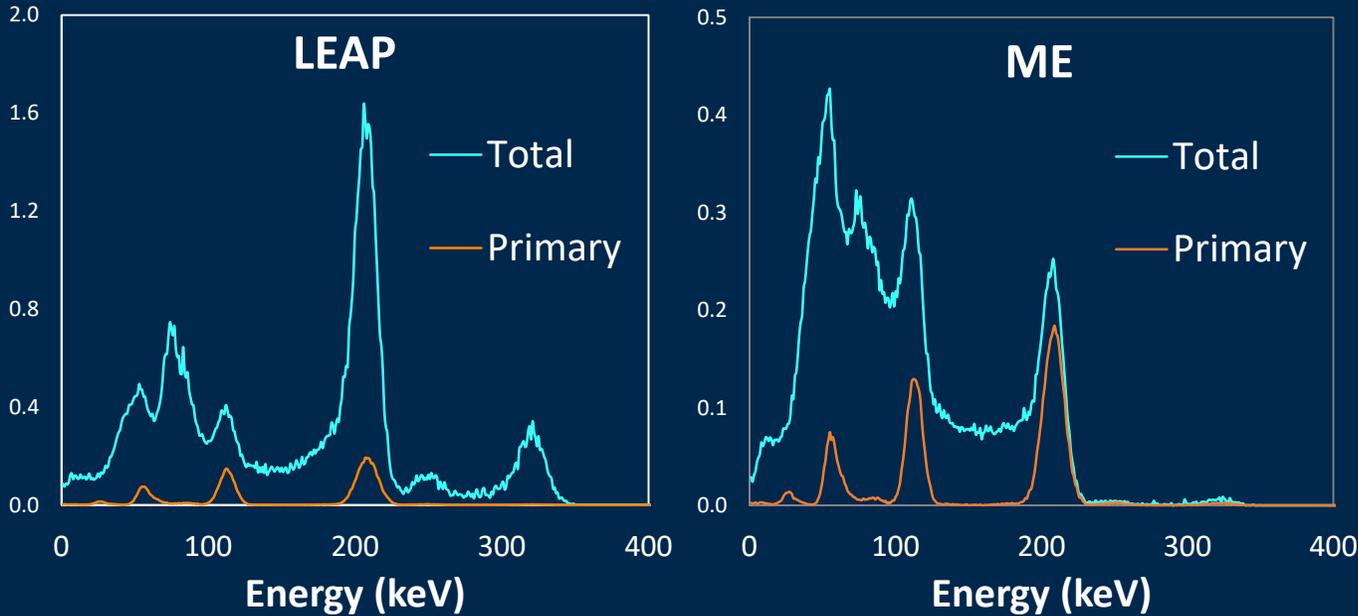
been used in radioimmunotherapy clinical trials to label different kinds of monoclonal antibodies (7–15).

There is a growing body of evidence that radionuclide therapy should follow patient-specific planning protocols, similar to those that are being routinely used in external-beam radiation therapy. Recent literature reviews show correlations between absorbed dose and tumor response as well as normal-tissue toxicity (16). Such correlations indicate that treatments should be based on personalized dosimetry, aiming to deliver therapeutically effective absorbed doses to tumors, while keeping doses to organs at risk below the threshold levels for deterministic adverse effects. In clinical PRRT studies, the primary adverse effects have been mainly renal and hematologic toxicities (2,6).

Although several studies have reported estimates of absorbed doses

# MIRD 26: Guidelines for SPECT

- Medium Energy Collimator, 208 keV photopeak window

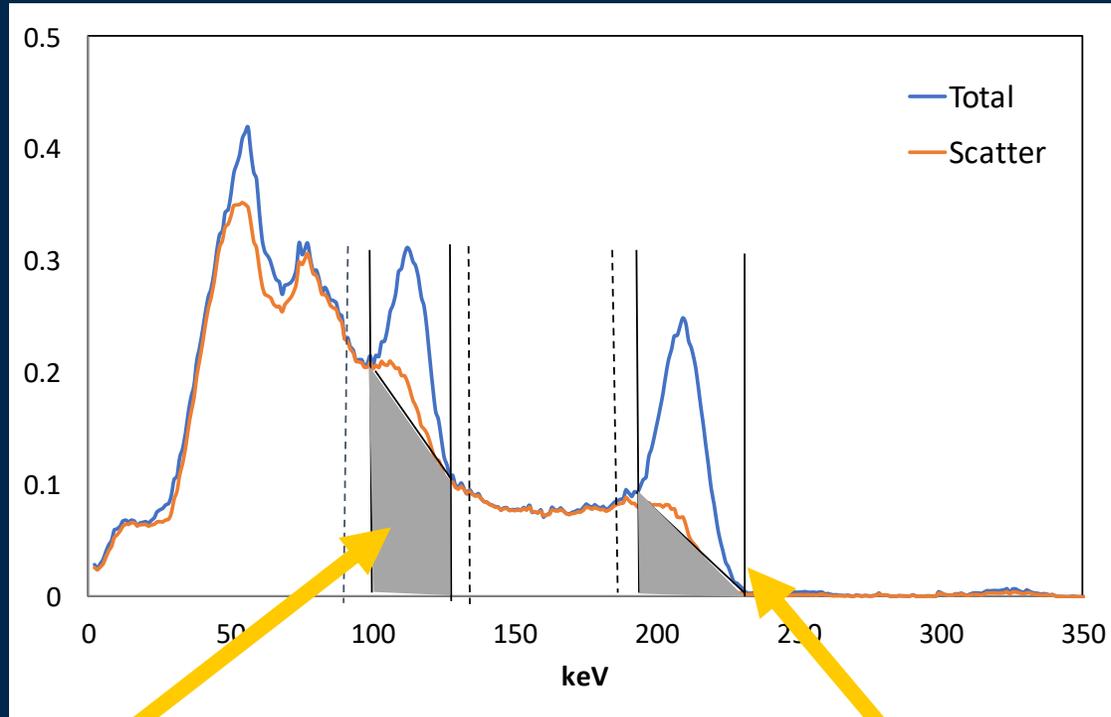


Ratios of Scattered Photons to Total Number of Photons Detected Within Energy Window (15% or 20%)

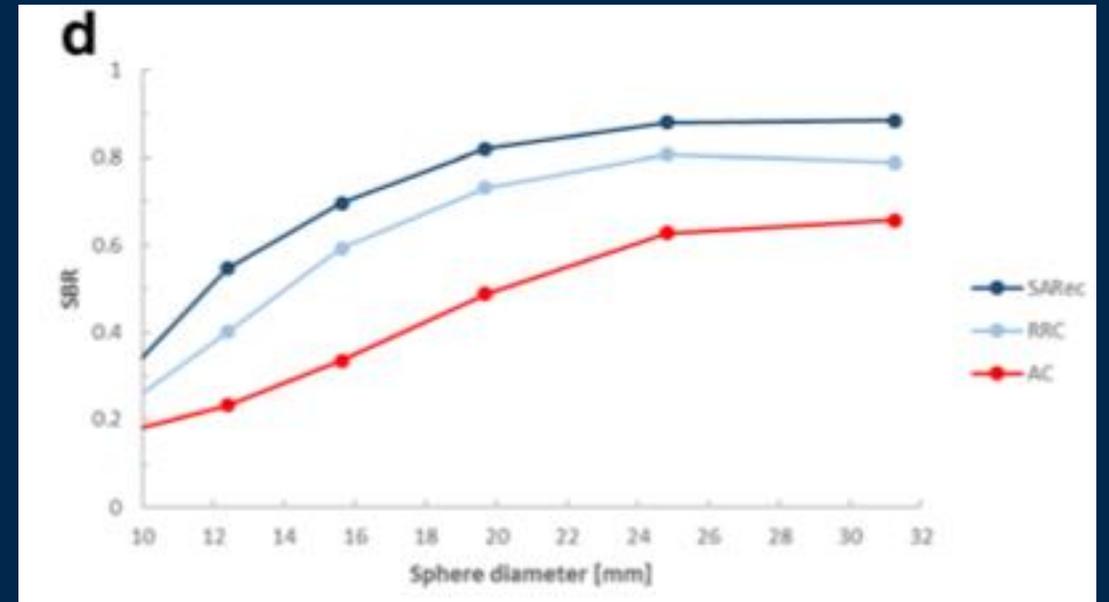
Crystal	Collimator*	113-keV window		208-keV window	
		15%	20%	15%	20%
3/8"	HE	0.60	0.55	0.27	0.22
3/8"	ME	0.60	0.55	0.27	0.22
3/8"	LEGP	0.53	0.49	0.21	0.18
3/8"	LEHR	0.49	0.47	0.20	0.17

# Scatter correction

- Triple Energy Window



- Monte Carlo based reconstruction
  - Improved recovery

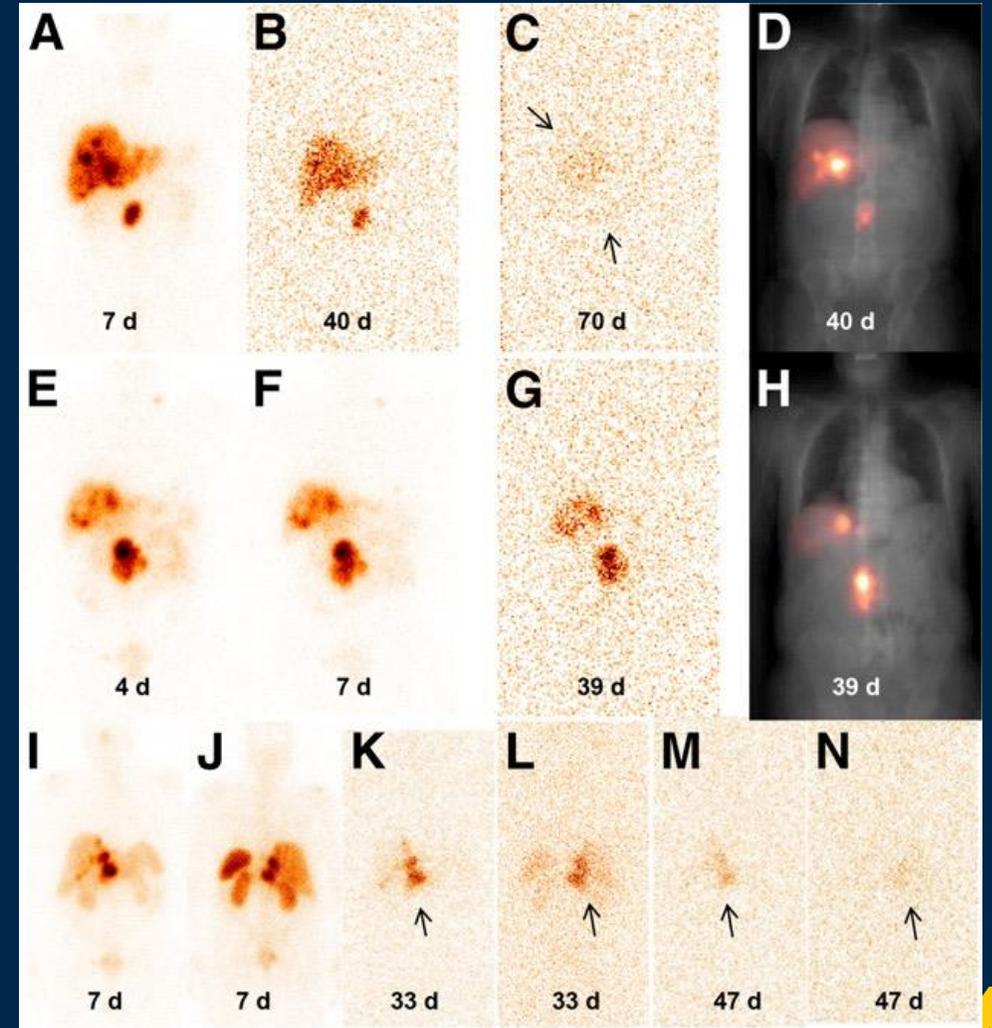


Use 3 windows when there is  
downscatter from higher peak  
Trapezoidal estimate of scatter

Don't need upper window  
when no downscatter  
Triangular estimate of scatter

# Long-term retention of Lu-177/Lu-177m

- Validity of extrapolating the 0 - 7 day time-activity fitted function to infinity
- 7 patients imaged at 5 - 7 weeks
  - Well visualized tumor uptake
  - Kidney uptake in 1 case
  - AD to WB and tumor 5 - 6% higher if later point is included
  - Tumor retention of Lu-177
  - Contribution from impurity Lu-177m negligible

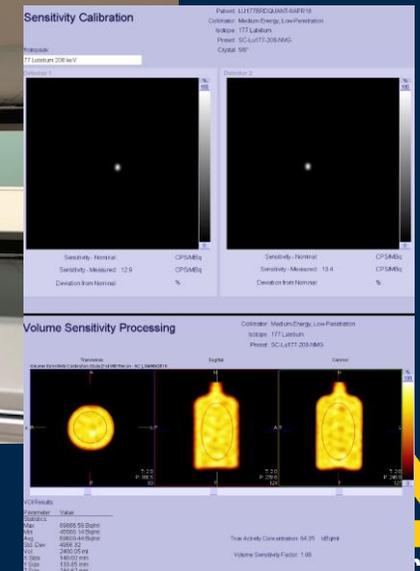
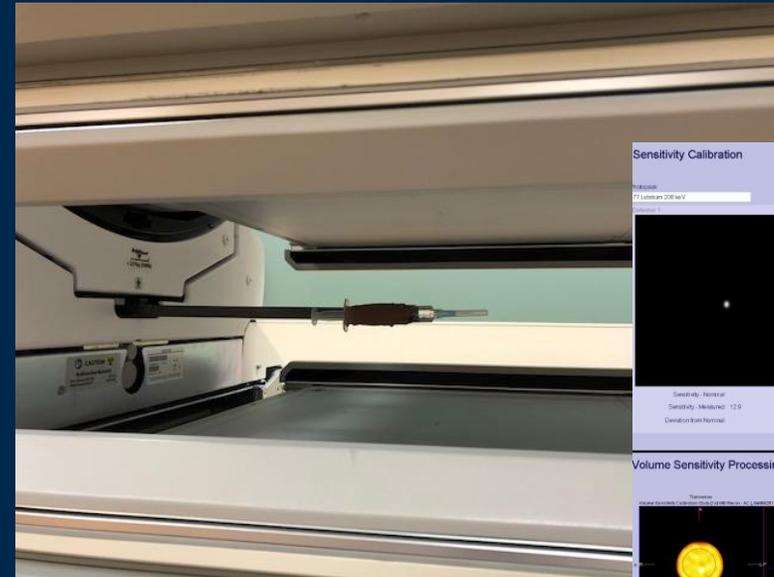


# Quantitative Lu-177

- xSPECT Calibration

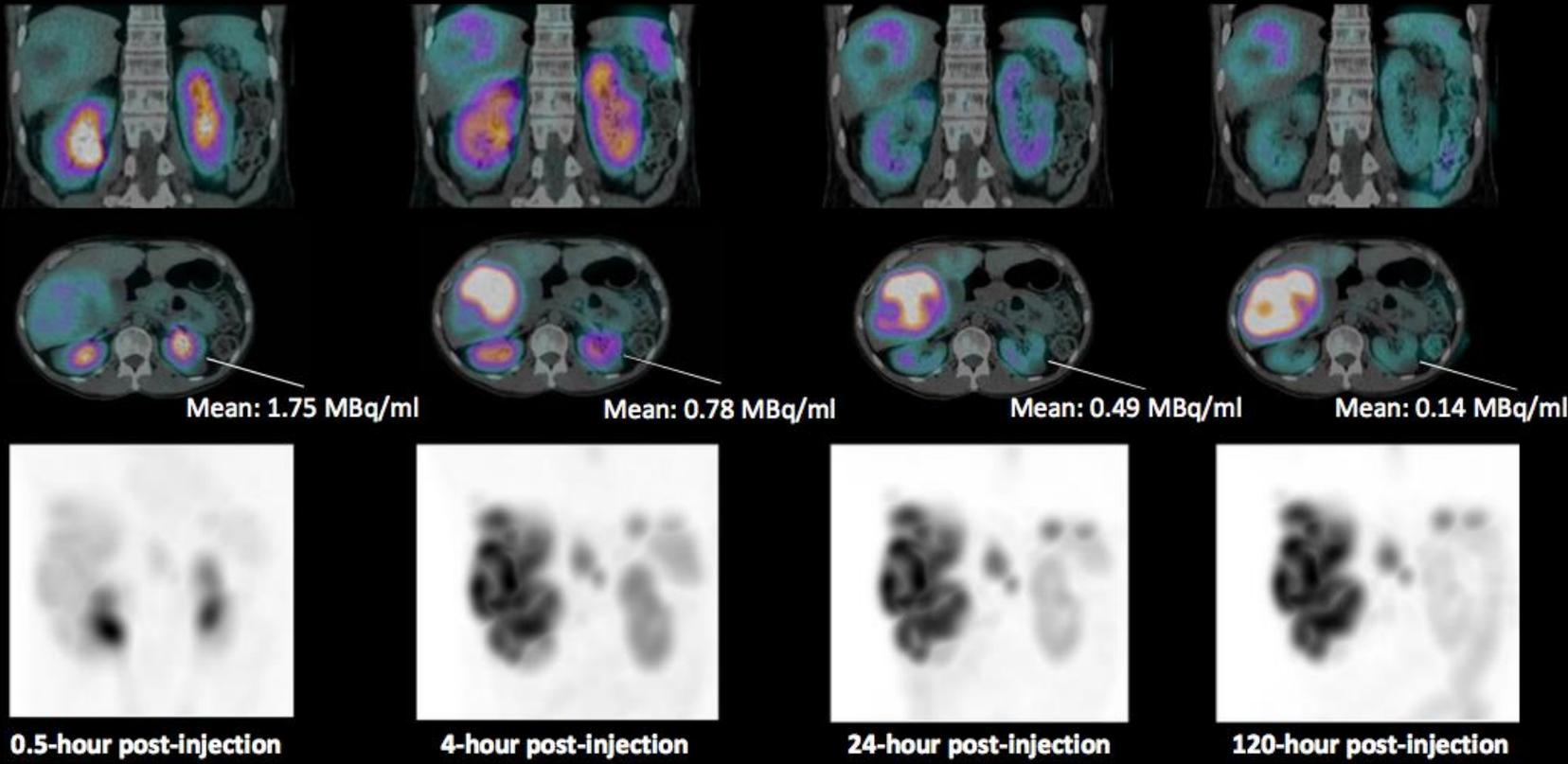


- 'Manual' Calibration



# Commercially available tools: XPECT Quant

## Sequential xSPECT Quant study following $^{177}\text{Lu}$ DOTATATE therapy in metastatic NET for dosimetry



## Dosimetry Research Tool



MIRD Organ Dose (Gy)	
Liver	4.86
Spleen	3.15
Left Kidney	3.73
Right Kidney	3.79
Hot Tumor 1	22.38

# Quantitative Lu-177 SPECT/CT Evaluation

## Optimizing Image Quantification for $^{177}\text{Lu}$ SPECT/CT Based on a 3D Printed 2-Compartment Kidney Phantom

Johannes Tran-Gia and Michael Lassmann

Department of Nuclear Medicine, University of Würzburg, Würzburg, Germany

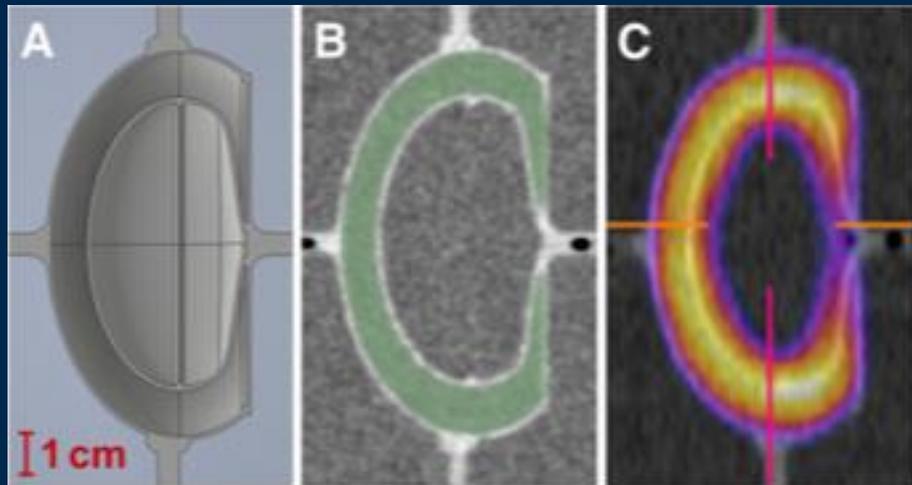
The aim of this work was to find an optimal setup for activity determination of  $^{177}\text{Lu}$ -based SPECT/CT imaging reconstructed with 2 commercially available methods (xSPECT Quant and Flash3D). For this purpose, 3-dimensional (3D)-printed phantoms of different geometries were manufactured, different partial-volume correction (PVC) methods were applied, and the accuracy of the activity determination

**Key Words:** radionuclide therapy; 2-compartment kidney phantom; 3D printing; partial volume correction; quantitative SPECT/CT; xSPECT Quant

**J Nucl Med 2018; 59:616–624**

DOI: 10.2967/jnumed.117.200170

With PVC, accuracy of activity in sphere, ellipsoid, cortex



# Commercially available software: GE Dosimetry Toolkit

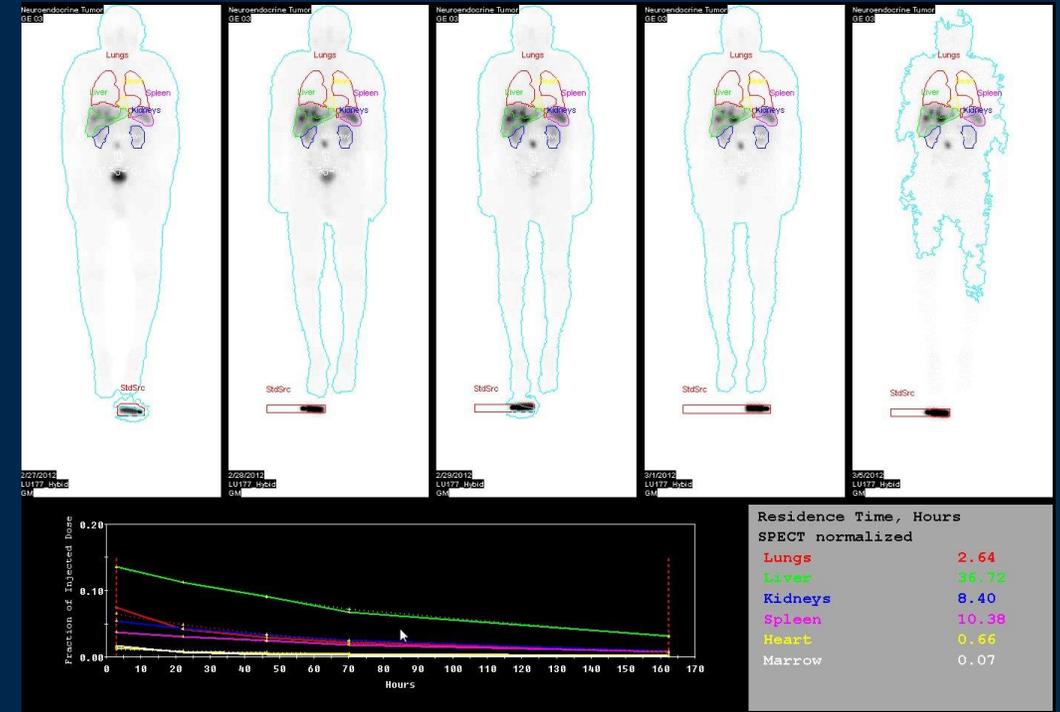
RESEARCH ARTICLE PLOS ONE | <https://doi.org/10.1371/journal.pone.0187570> November 6, 2017

## Software-assisted dosimetry in peptide receptor radionuclide therapy with <sup>177</sup>Lutetium-DOTATATE for various imaging scenarios

Dennis Kupitz<sup>1\*</sup>, Christoph Wetz<sup>1</sup>, Heiko Wissel<sup>1</sup>, Florian Wedel<sup>2</sup>, Ivayla Apostolova<sup>1,3</sup>, Thekla Wallbaum<sup>1</sup>, Jens Ricke<sup>1,4</sup>, Holger Amthauer<sup>1,2</sup>, Oliver S. Grosser<sup>1</sup>

<sup>1</sup> Department of Radiology and Nuclear Medicine, University Hospital Magdeburg A.ö.R., Otto-von-Guericke University Magdeburg, Magdeburg, Germany, <sup>2</sup> Department of Nuclear Medicine, Charité—

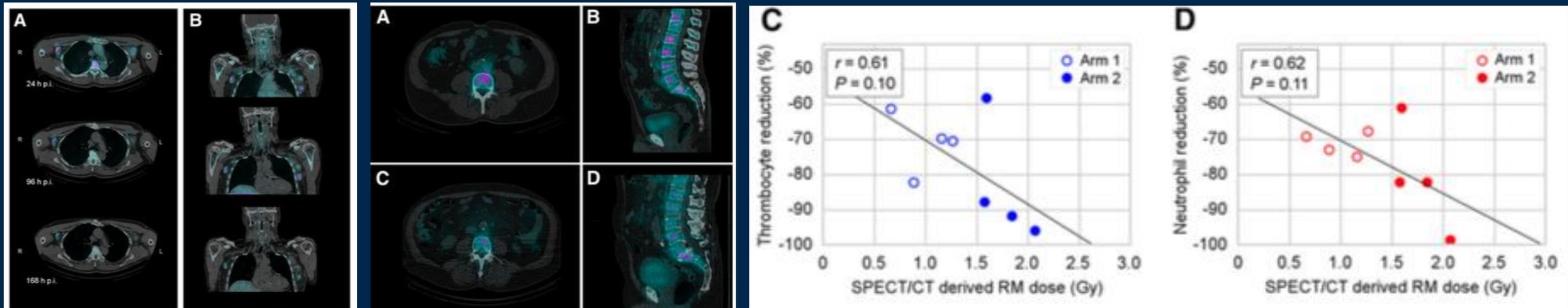
- Analysis using GE Dosimetry Toolkit coupled with OLINDA
  - Quantification, registration, segmentation, time-activity fit
  - Compared Multi SPECT/CT, WB only and hybrid WB -SPECT/CT



	Absorbed dose per admin. activity (Gy per GBq)		
	Multi SPECT/CT	Hybrid	Planar
Lesions	2.58 ± 1.47	3.09 ± 2.16	5.32 ± 6.26
Kidney	0.48 ± 0.18	0.59 ± 0.30	0.76 ± 0.43

# SPECT/CT based dosimetry in Lu-177 Lilotomab RIT of NHL

- 8 patients, SPECT/CT at 24, 96, 168 h
  - Tumor dosimetry using OLINDA sphere model
  - Imaging (lumbar vertebrae) based bone marrow dosimetry
- Median tumor absorbed dose 264 cGy (range 75 - 794 cGy)
- Red marrow dose 57 to 208 cGy
  - Statistically significant dose-toxicity (not with blood-based calc.)



# Why patient specific dosimetry? Trial at Lund University

Eur J Nucl Med Mol Imaging (2017) 44:1480–1489  
DOI 10.1007/s00259-017-3678-4



ORIGINAL ARTICLE

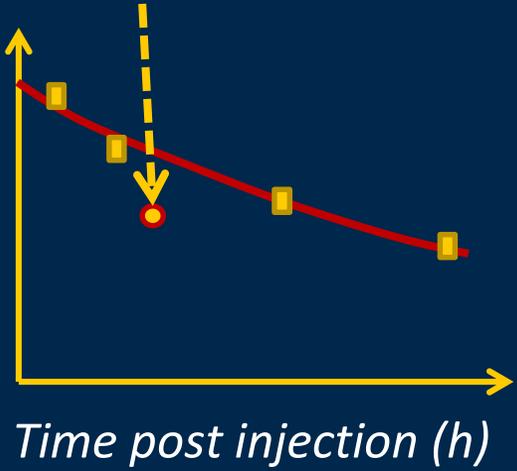
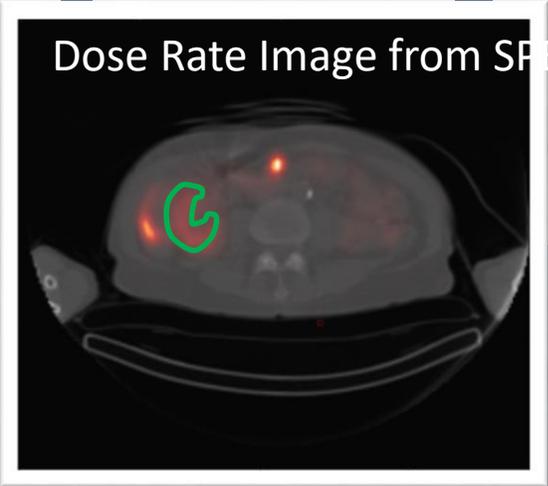
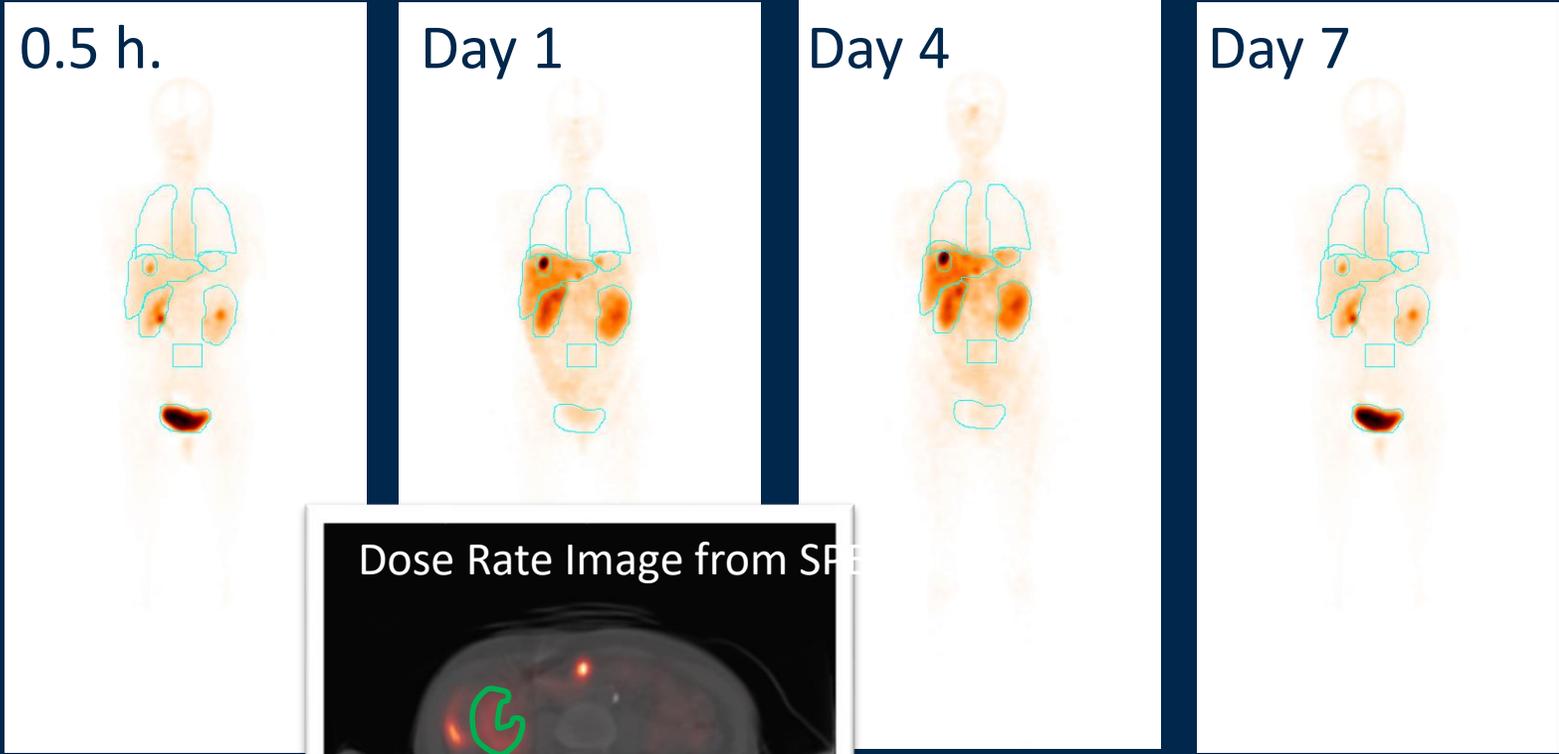
## Individualised $^{177}\text{Lu}$ -DOTATATE treatment of neuroendocrine tumours based on kidney dosimetry

Anna Sundlöv<sup>1,2</sup>  • Katarina Sjögren-Gleisner<sup>3</sup> • Johanna Svensson<sup>4</sup> •  
Michael Ljungberg<sup>3</sup> • Tomas Olsson<sup>2</sup> • Peter Bernhardt<sup>5,6</sup> • Jan Tennvall<sup>1,2</sup>

- Treatment based on renal dosimetry
- 51 patients with NET
- Purpose was to give as many standard (7.4 GBq) cycles keeping kidney BED < 27 Gy
- Detailed dosimetry using hybrid planar/SPECT approach

# Lu-177 DOTATATE trial at Lund Univ.: Hybrid Planar/SPECT

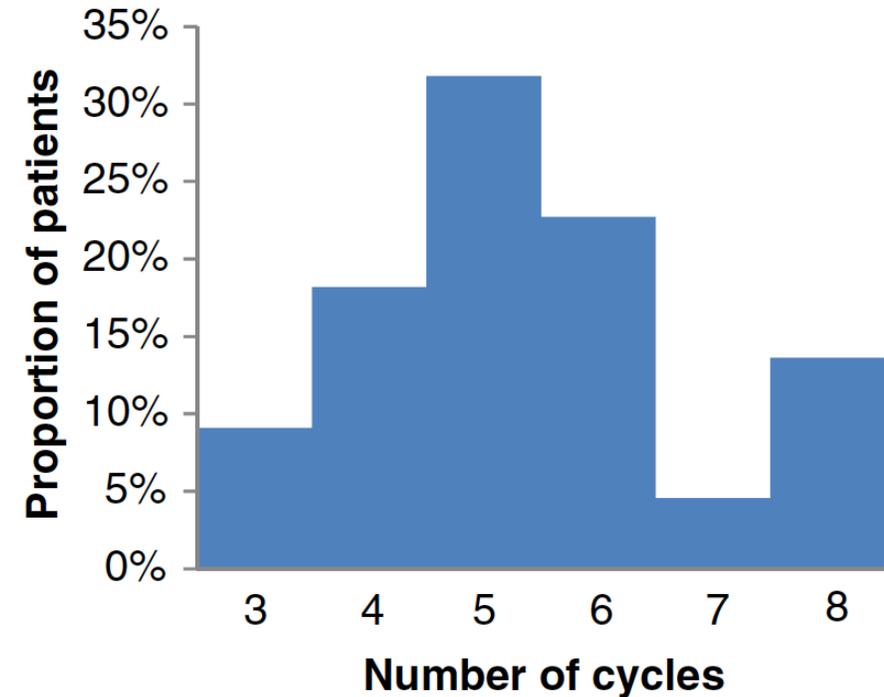
## Co-registered whole-body images



Courtesy of Michael Ljungberg, Lund University Sweden

# Why Patient Specific Dosimetry? Lund Univ. Trial

- Treatment based on renal dosimetry
  - Considerable variation in number of cycles.
    - Median 5 cycles, range 3 - 7
    - No Grade 3-4 toxicity
    - Absorbed dose/cycle varied between patients and between cycles for the same patient
- Highlights the value of individualized dosimetry



**Fig. 3** Frequency distribution of number of cycles delivered within the protocol-specified BED-limits

# Why patient specific dosimetry?

ACTA ONCOLOGICA, 2018  
VOL. 57, NO. 4, 516-521  
ACTA ONCOLOGICA, 2018  
VOL. 57, NO. 4, 516-521  
<https://doi.org/10.1080/0284186X.2017.1378431>



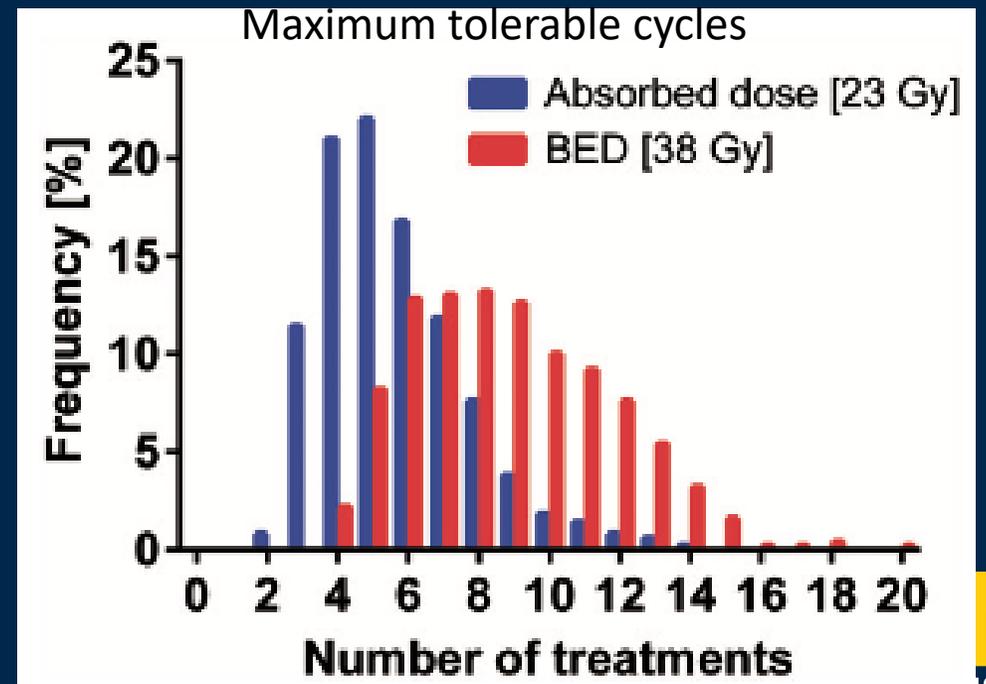
ORIGINAL ARTICLE

**Kidney dosimetry during  $^{177}\text{Lu}$ -DOTATATE therapy in patients with neuroendocrine tumors: aspects on calculation and tolerance**

Mattias Sandström<sup>a,b</sup>, Ulrike Garske-Román<sup>a</sup>, Silvia Johansson<sup>c</sup>, Dan Granberg<sup>d</sup>, Anders Sundin<sup>a</sup> and Nanette Freedman<sup>e,f</sup>

- 500 patients: SPECT/CT and WB imaging at 1,4,7 d after cycle 1. Assumed same AD from all cycles
- Considerable variation in AD, BED  
AD 4.4 (1.7-9.8), 4.2 Gy (1.1-9.8)  
BED 4.7(1.7-11.6), 4.4Gy (1.0-11.8)  
for R & L kidney

- With BED limit of 38 Gy to kidney and AD limit of 2 Gy to marrow 95% could get > 4 cycles with only 0.5% reaching limit at 3 cycles.

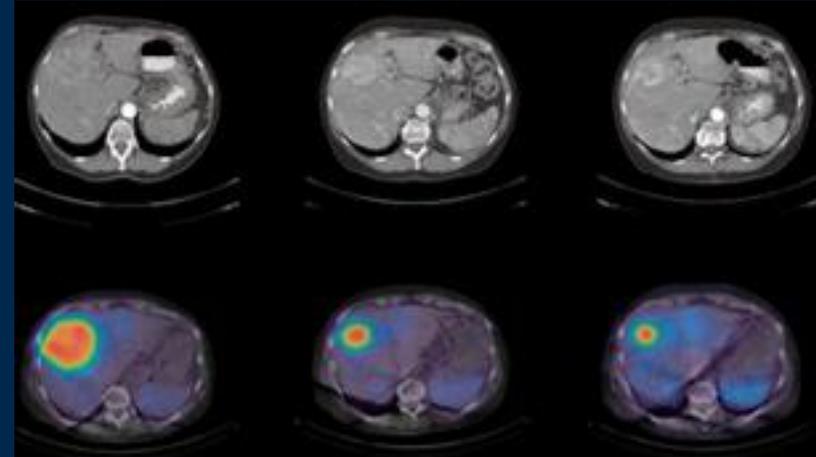


# Why Patient Specific Dosimetry? Tumor dose-response

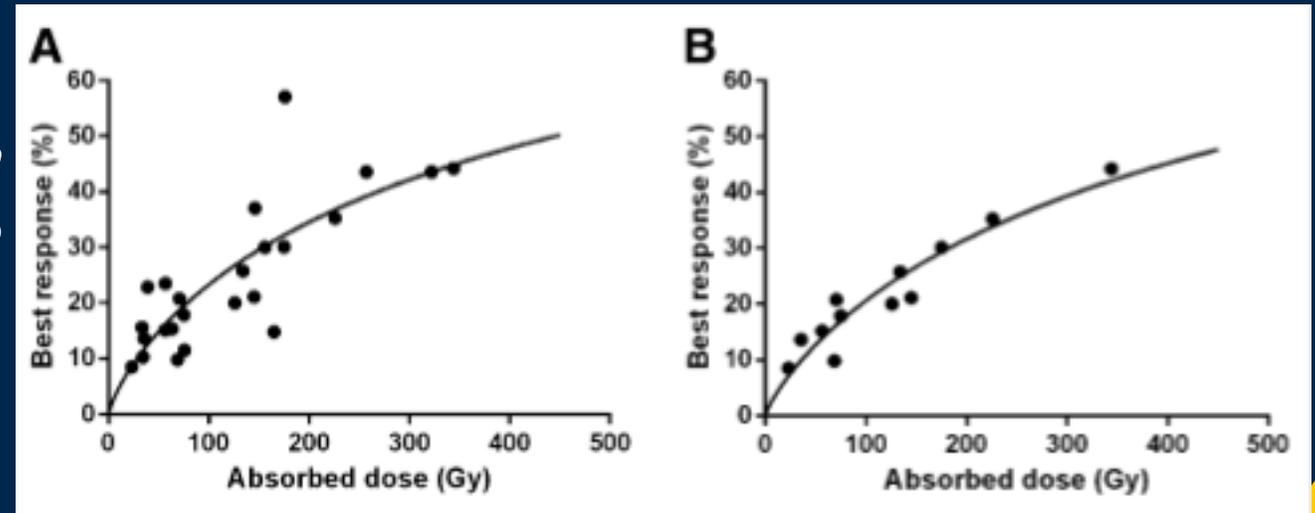
## Dose Response of Pancreatic Neuroendocrine Tumors Treated with Peptide Receptor Radionuclide Therapy Using $^{177}\text{Lu}$ -DOTATATE

Ezgi Ilan<sup>1,2</sup>, Mattias Sandström<sup>1,2</sup>, Cecilia Wassberg<sup>1,3</sup>, Anders Sundin<sup>1,3</sup>, Ulrike Garske-Román<sup>1,3</sup>, Barbro Eriksson<sup>4</sup>, Dan Granberg<sup>4</sup>, and Mark Lubberink<sup>1,2</sup>

*J Nucl Med* 2015; 56:177–182



- 24 lesions (> 2.2 cm)
- Sequential SPECT/CT at 24, 96, 168 h after some cycles
- PVC, no SC, OLINDA AD calculation (self-dose)



# Simplification of procedure: single time point dosimetry

## Dose Mapping After Endoradiotherapy with $^{177}\text{Lu}$ -DOTATATE/DOTATOC by a Single Measurement After 4 Days

Heribert Hänscheid<sup>1</sup>, Constantin Lapa<sup>1</sup>, Andreas K. Buck<sup>1</sup>, Michael Lassmann<sup>1</sup>, and Rudolf A. Werner<sup>1,2</sup>

- Presented the theory to show that dose can be estimated within reasonable accuracy from a single measurement post-administration

Time integral  $\sim u(r_s, t_1) * 2 * t_1 / \ln(2)$

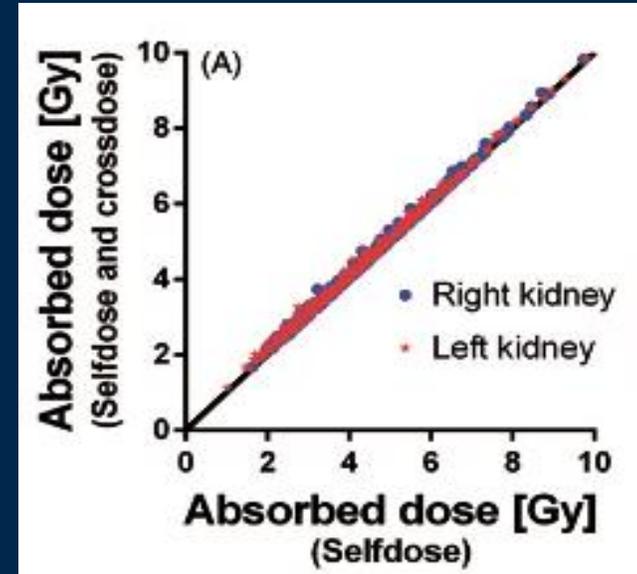
Single meas. at  $t_1$

- Planar imaging of 29 patients at 4, 24, 38 and 96 h with mono and bi-exponential fits
- Deviations of the approx. from the 'true' time integral for  $t_1 = 24, 48, 72, 96, 120, 144$  h

Tissue	Quantile	$\bar{u}(r_s, t_i) / \bar{u}(r_s) - 1$					
		24 h	48 h	72 h	96 h	120 h	144 h
Kidneys	1 (maximum)	-18%	+17%	+25%	+17%	+7%	+7%
	0.9	-24%	+9%	+16%	+10%	+2%	-7%
	0.5 (median)	-33%	0%	+6%	+5%	-5%	-18%
	0.1	-40%	-8%	+4%	-3%	-16%	-31%
	0 (minimum)	-61%	-33%	-15%	-9%	-25%	-41%
Liver	1 (maximum)	-33%	-1%	+10%	+12%	+10%	+6%
	0.9	-37%	-6%	+7%	+9%	+8%	+5%
	0.5 (median)	-43%	-11%	+4%	+6%	+3%	-1%
	0.1	-52%	-21%	-4%	+3%	-1%	-11%
	0 (minimum)	-64%	-38%	-20%	-7%	-4%	-12%
Spleen	1 (maximum)	-31%	+3%	+20%	+20%	+17%	+13%
	0.9	-38%	-2%	+12%	+15%	+12%	+8%
	0.5 (median)	-44%	-12%	+5%	+8%	+6%	+1%
	0.1	-53%	-22%	-4%	+5%	+3%	-7%
	0 (minimum)	-58%	-27%	-9%	+2%	-4%	-16%
NET	1 (maximum)	-36%	-1%	+15%	+16%	+11%	+10%
	0.9	-40%	-6%	+8%	+10%	+10%	+7%
	0.5 (median)	-49%	-17%	0%	+6%	+5%	+5%
	0.1	-60%	-32%	-13%	-2%	+2%	-6%
	0 (minimum)	-67%	-43%	-24%	-11%	-3%	-14%

# Simplification of procedure: ignore cross dose?

- How important is cross dose for Lu-177?
  - Betas have short path length, gammas have low intensity
- Kidney self-dose 4.2 Gy(1.0-9.8), cross-dose 0.1Gy(0.0-0.5)



cross-dose  
< 10% in  
97% of patients

- 500 patients with NETs treated with Lu-177 DOTATATE
  - Kidney self dose from SPECT/CT at 1, 4, 7 d.
  - Cross dose from WB imaging and OLINDA dose factors

- Important for tumor?
  - Simulation study showed minimal differences between MC and local energy absorption

# Simplification of procedure: AD vs. BED ?

- BED was calculated as

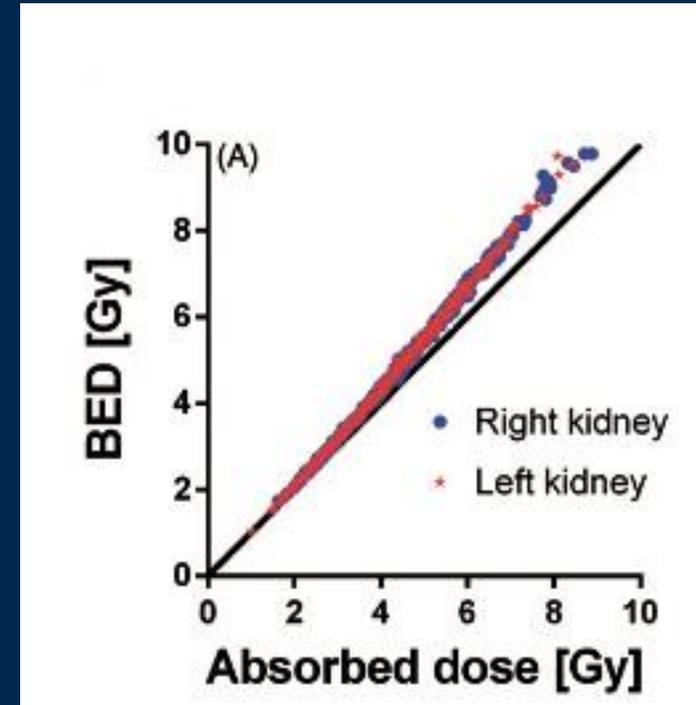
$$BED = \sum_i D_i + \frac{\beta}{\alpha} \frac{t_{1/2}^{rep}}{t_{1/2}^{rep} + t_{1/2}^{eff}} \sum_i D_i^2$$

- $D_i$  is absorbed dose for cycle  $i$
- $\alpha/\beta = 2.6$  Gy and  $t_{rep} = 2.8$  h

- Results should be considered as approximations

- $\alpha/\beta$  not specific to kidney and PRRT

- 500 patients: BED only slightly higher than AD. Difference increases with absorbed dose



- But ...

# Simplifications?

## Patient-Specific Dosimetry in Predicting Renal Toxicity with $^{90}\text{Y}$ -DOTATOC: Relevance of Kidney Volume and Dose Rate in Finding a Dose–Effect Relationship

J Nucl Med 2005; 46:99S–106S

Raffaella Barone, MD<sup>1</sup>; Françoise Borson-Chazot, MD, PhD<sup>1</sup>; Roelf Valkema, MD, PhD<sup>2</sup>; Stéphan Walrand, PhD<sup>1</sup>;

- ‘The use of a **refined absorbed dose methodology** led to the finding of a clear kidney dose-response relationship in patients treated with  $^{90}\text{Y}$ -DOTATOC. Our data provide evidence that **patient-specific anatomy** and **dose-rate effects** cannot be neglected. The BED model appears to be a reliable predictor of toxicity and could thus be helpful in implementation of individual treatment planning’

Thank You

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