



Dosimetry Needs and Methods for SRT: Yttrium-90

Yuni Dewaraja, Emilie Roncali, Mark Madsen

Department of Radiology
University of Michigan

University of California, Davis; University of Iowa

NCI Workshop on Dosimetry of Systemic Radiopharmaceutical Therapy (SRT) Rockville, MD, April 19-20, 2018

Disclosures

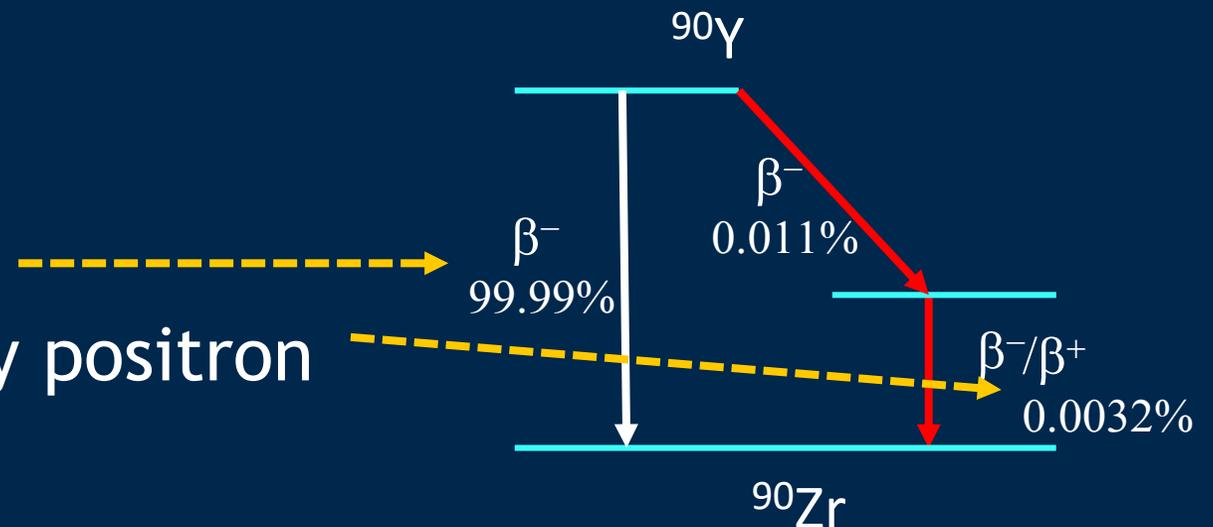
- Yuni Dewaraja is a consultant for MIM Software, Inc.

^{90}Y Imaging/Dosimetry

- Almost pure beta emitter
 - $E_{\text{ave}} = 0.94 \text{ MeV}$; mean tissue penetration=2.5 mm; $T_{1/2}=64 \text{ h}$
 - Betas can eradicate tumor cells that are not directly targeted
 - ^{90}Y microsphere RE, ^{90}Y ibritumomab, ^{90}Y DOTATOC PRRT

- Imaging: complex

- SPECT via bremsstrahlung
- PET via very low probability positron



- Absorbed dose calculation: relatively easy

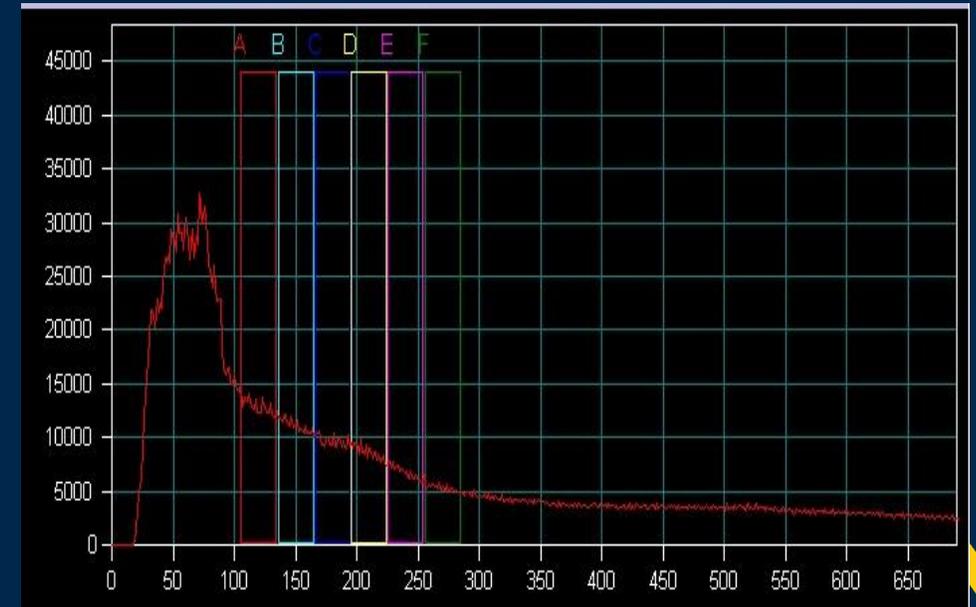
- Under certain conditions can assume local energy deposition
 - lack of γ and range of β relative to SPECT/PET resolution

Bremsstrahlung imaging

- Challenges
 - Inefficient: $< 4\%$ of β tissue interactions give photons $> 50\text{keV}$
 - Not suitable for pre-therapy tracer imaging
 - Continuous bremsstrahlung spectrum extending to 2.1 MeV
 - Penetration (downscatter) of high energy photons
 - Tissue dependent bremsstrahlung generation probabilities
 - Yield not same in tissue vs. bone
- Internal bremsstrahlung
 - Photons emitted during the β decay process itself

Bremsstrahlung SPECT Imaging: Guidelines

- HE collimator
- Acquisition window
 - Within 100 - 500 keV
 - 100 - 200 keV (avoids x-ray, optimal primary-to-scatter)
- Single (narrow) window vs. multi window reconstruction model
- Model/Monte Carlo based SC
 - Energy window based not suitable with continuous spectrum



Bremsstrahlung SPECT/CT Reconstruction with Scatter Correction

- **Model based**

Minarik et al, Phy Med Biol 2008; Rong et al, Med Phys 2012

- Pre-calculated scatter kernels

- **Fully Monte Carlo**

Elschot et al, JNM 2013

- MC reconstruction with 'on the fly' calculation of SC and AC

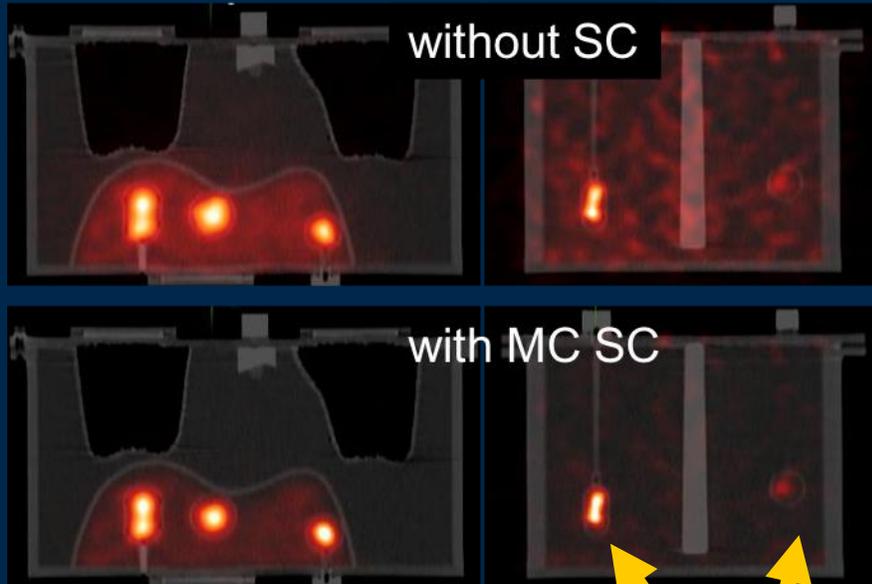
- **Monte Carlo generated scatter estimate**

Dewaraja et al, Med Phys 2017

- Less computationally demanding than fully MC

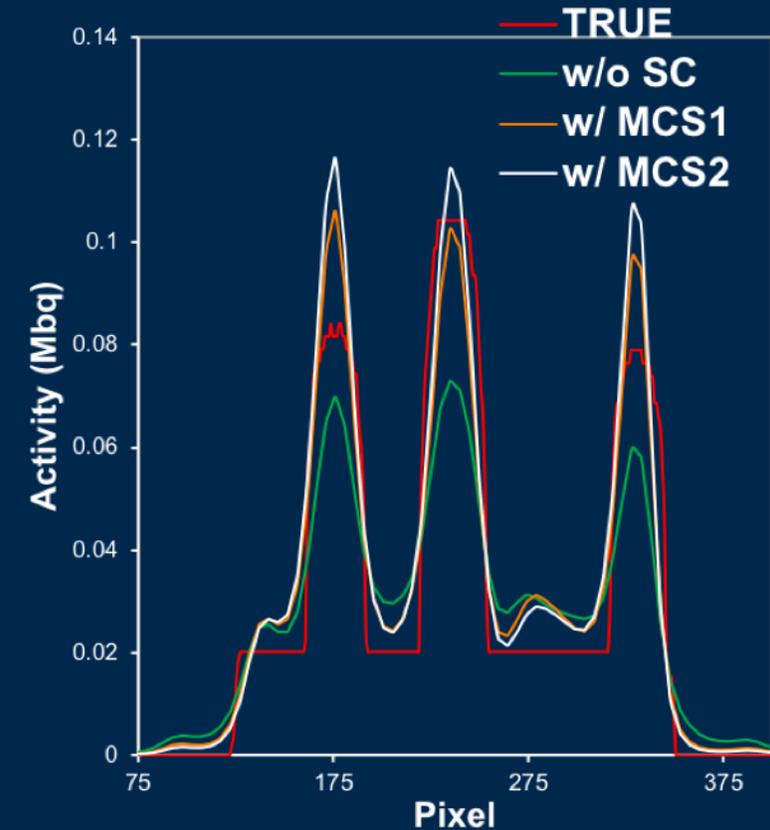
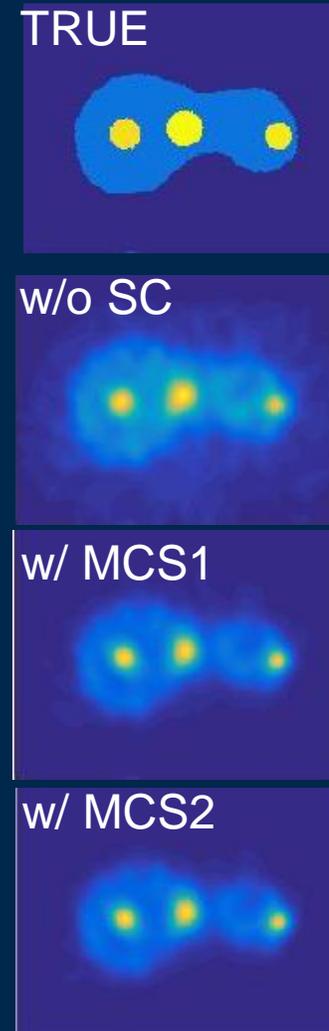
Y-90 SPECT: Impact of scatter correction

- Improved visibility

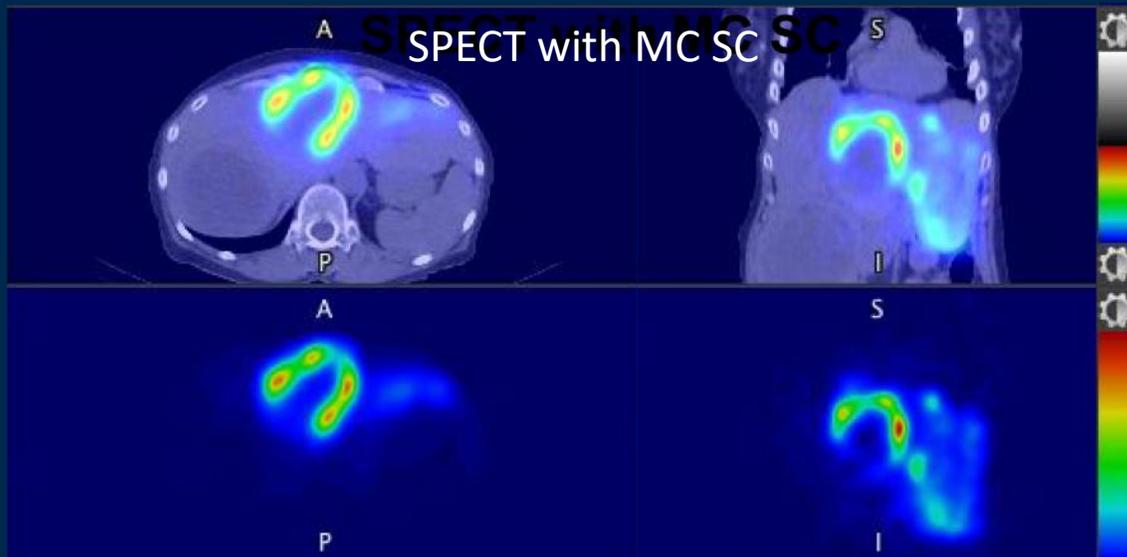
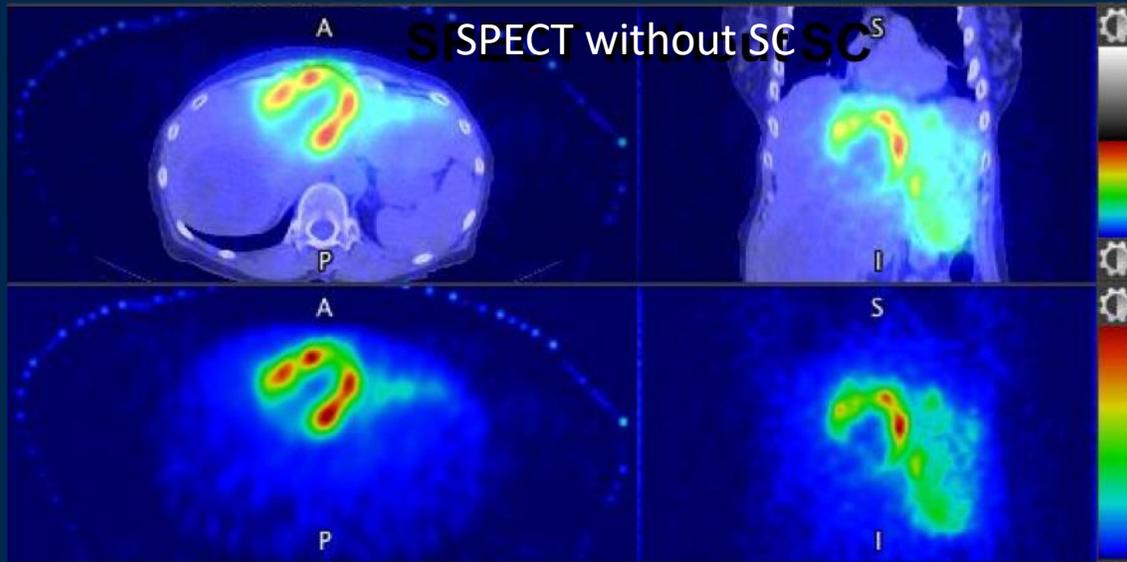


Visibility of low uptake objects important for detecting extra hepatic deposition

- Improved contrast/quantification



Impact of scatter correction: RE patient example



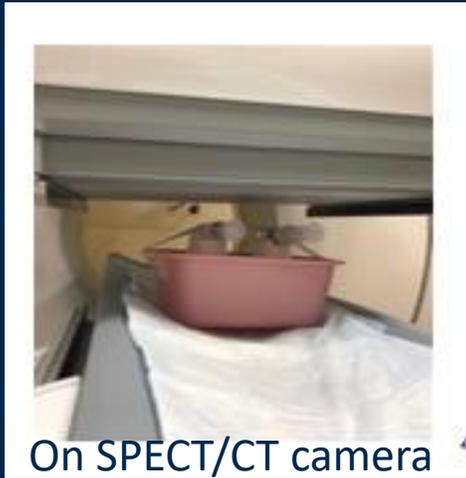
In 11 lesions (5 patients) without and with MC SC
Mean lesion uptake was 4.9 vs. 7.1 MBq/mL
Mean normal liver uptake was 1.6 vs. 1.5 MBq/mL
Lesion-to-liver uptake ratio was 2.7 vs. 4.3 (P=0.040)

Tissue dependent bremsstrahlung generation probabilities

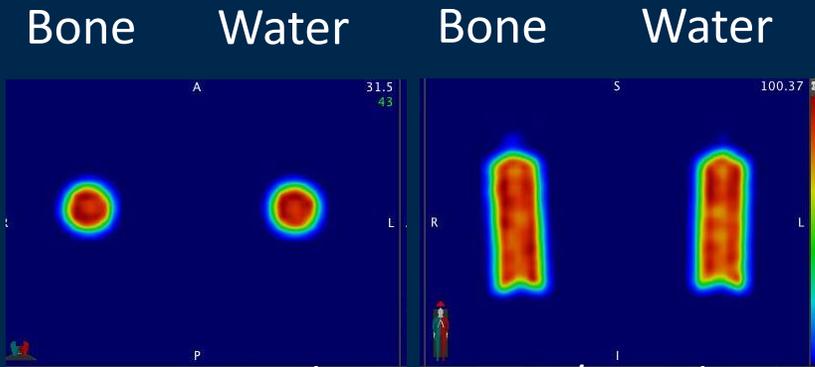
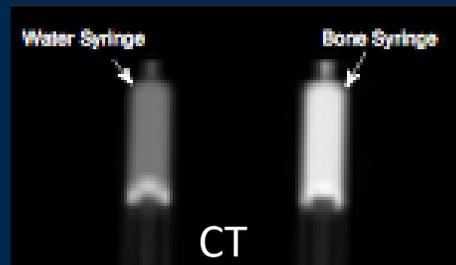
- Bremsstrahlung **yield** $\propto Z^2$
 - Same activity in different tissue will produce different number of photons
 - Impact quantification of heterogeneous tissue
- Yield in bone is 1.5 - 2 times that of tissue
- Can account for this by incorporating probabilities in the reconstruction system matrix and using CT to determine voxel composition

Demonstrating tissue dependent bremsstrahlung yield

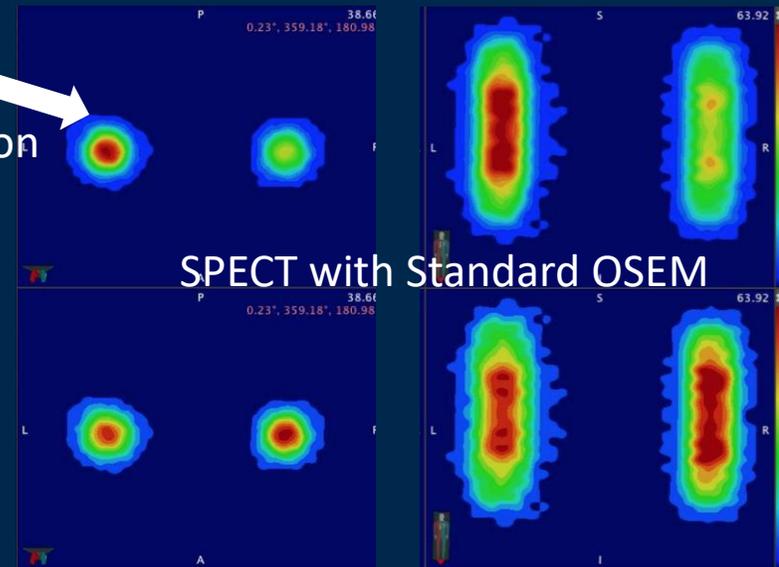
Same Y-90 conc in 2 syringes with bone equiv. liquid (potassium salt) & water



Bone 1.5 times more intense although same Y-90 concentration

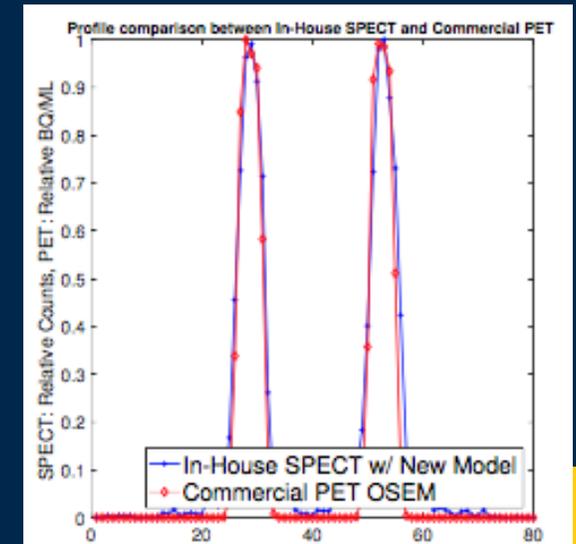
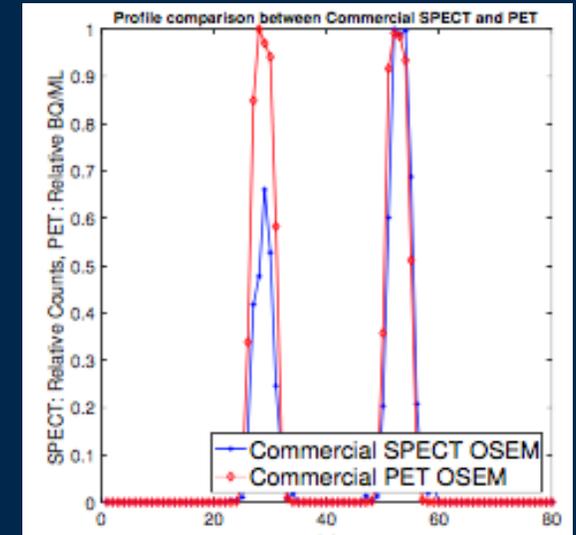


PET (consistent w/ TRUE)



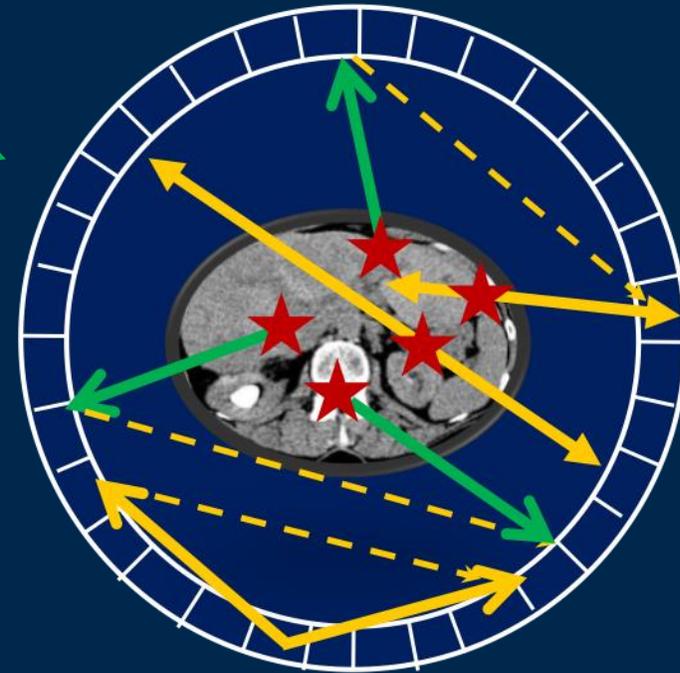
SPECT with Standard OSEM

SPECT with new system matrix (consistent w/ TRUE)



Y-90 PET

- Very low probability positron (low true coincidences) in the presence of bremsstrahlung (high random coincidences)
- Poor image quality
 - Improved with time-of-flight



Y-90 SPECT vs PET

- SPECT: higher visibility lower resol.
- PET: higher resolution, high noise

Patient specific dosimetry in Y-90 radioembolization

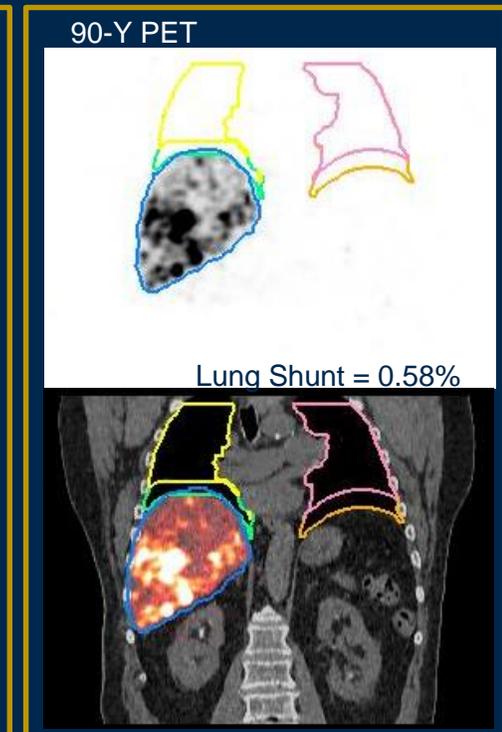
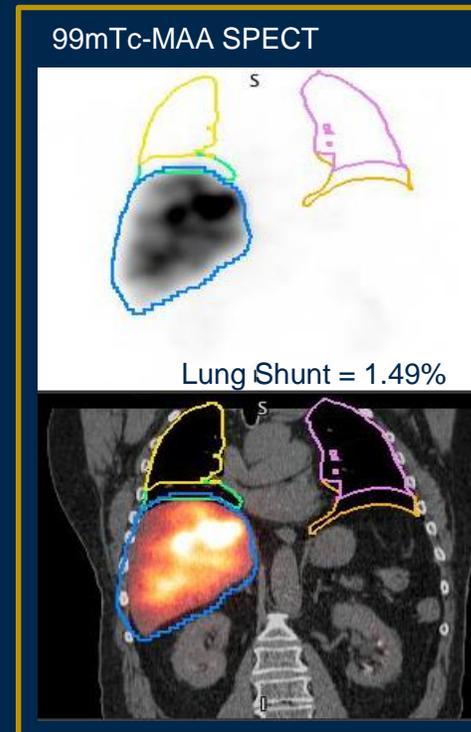
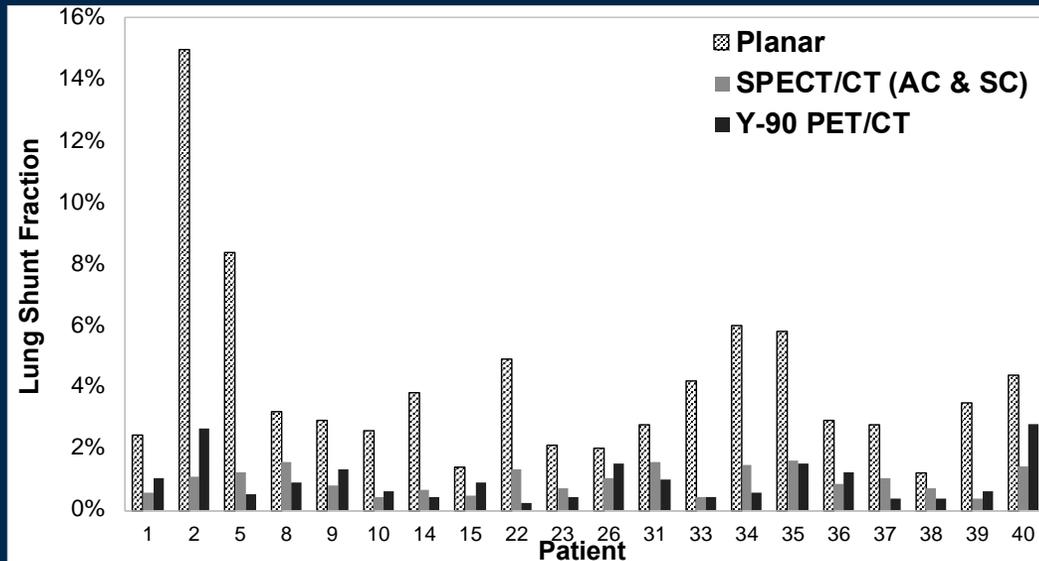
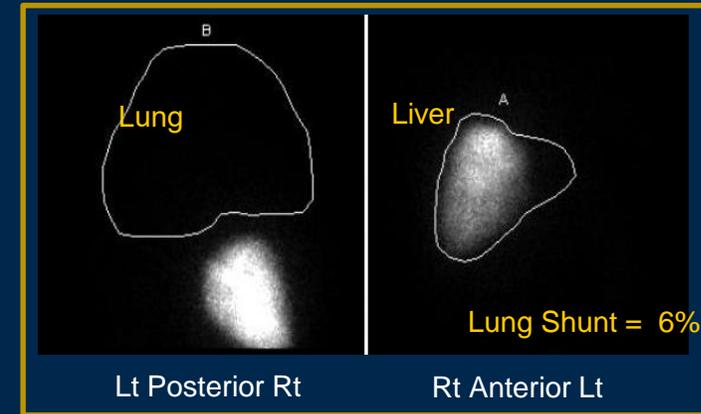
- Need only a single imaging point to get time-integrated activity
- Voxel level dosimetry can be based on local energy deposition
- Pre-therapy ^{99m}Tc -MAA SPECT/CT study for better planning ?
 - Currently mostly used to assess extra-hepatic deposition
 - Differences between MAA and microsphere distribution
- Post therapy Y-90 PET and SPECT can be used for
 - Safety, dose verification (immediate prediction of response)
 - Establishing lesion dose - response, normal liver dose-toxicity

Y-90 RE: Initial results from ongoing study at U Michigan

- Methods to improve Y-90 post therapy imaging
 - Dewaraja et al. Improved quantitative 90Y bremsstrahlung SPECT/CT reconstruction with Monte Carlo scatter modeling. *Med Phys.* 2017;44:6364-6376.
 - Lim H, Dewaraja Y, Fessler J. A PET reconstruction formulation that enforces non-negativity in projection space for bias reduction in Y-90 imaging. *Phys Med Biol* 2018
- Dosimetry based on Tc-MAA SPECT/CT, Y-90 SPECT/CT & PET/CT
 - Patients with HCC or liver mets treated with glass microspheres
 - Radiologist defined lesions, 3D dosimetry using DPM MC code
- Follow up for dose - outcome
 - RECIST, mRECIST, liver function tests

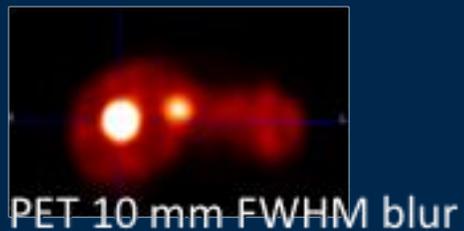
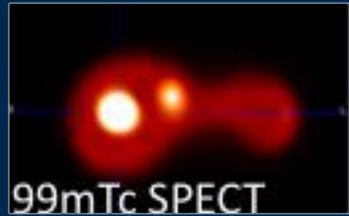
Value of Tc-MAA SPECT/CT for Lung Shunt Estimation

- Planar calculation, used in clinic, overestimates LS
- SPECT/CT based
 - Higher accuracy
 - Auto liver/lung contouring
 - Less variability

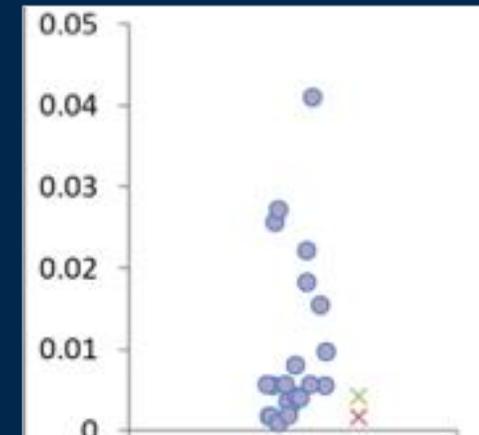
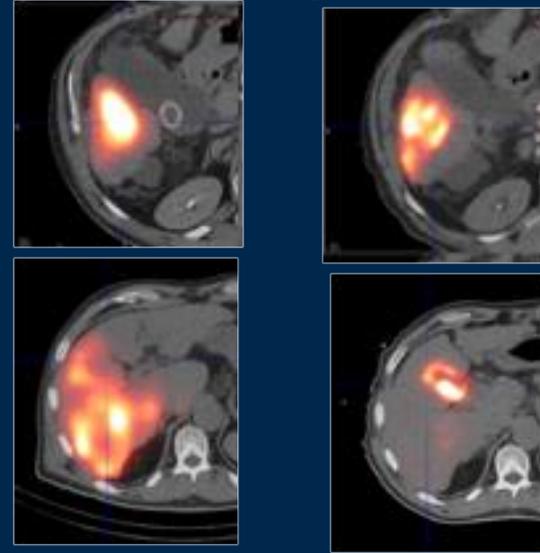


Tc-99m MAA SPECT vs Y-90 PET spatial concordance

- Phantom: good spatial concordance



- Patients: poor concordance

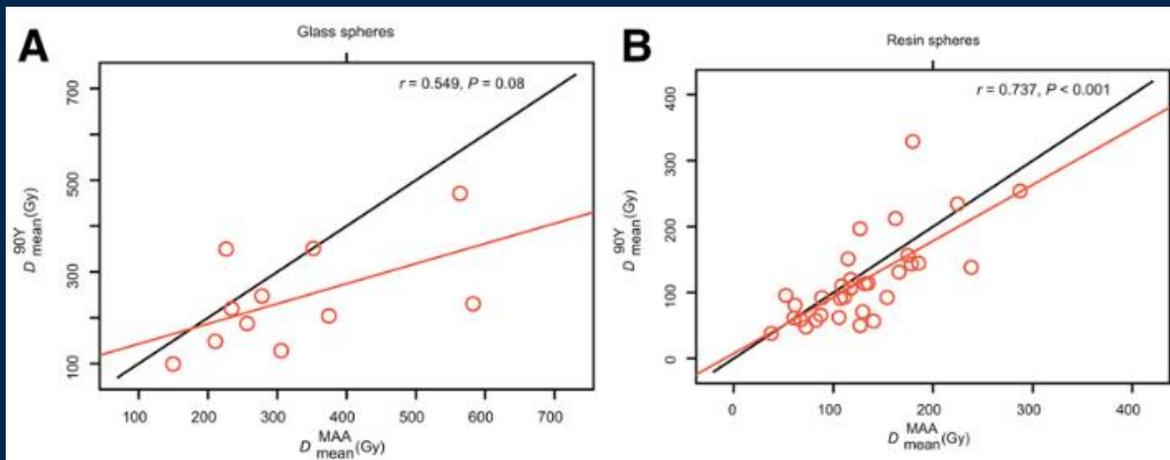


Tc-MAA predicted vs. Y-90 delivered mean absorbed dose

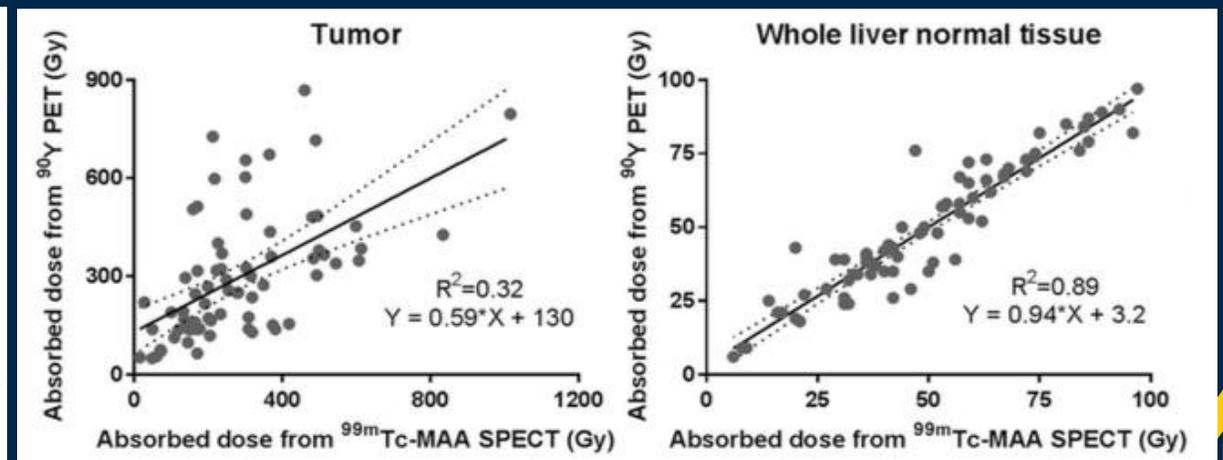
Past studies looking at Tc MAA - Y90 concordance

- Mixed conclusions

	Spatial granularity	registration	device	Analysis	90Y	Cath tip info?	
Wondergem et al JNM 2013	segment	?	resin	BlandAlt	SPECT	Y	Poor correlation
Gnesin et al JNM 2016	tumor	?	mix	ccc of dose ratio mean, D70	PET	N	moderate
Kneusarek et al TCRT 2010	Voxel-level	CT-CT	resin	Correlation coefficient, L2 norm	SPECT	N	Poor to highly correlated

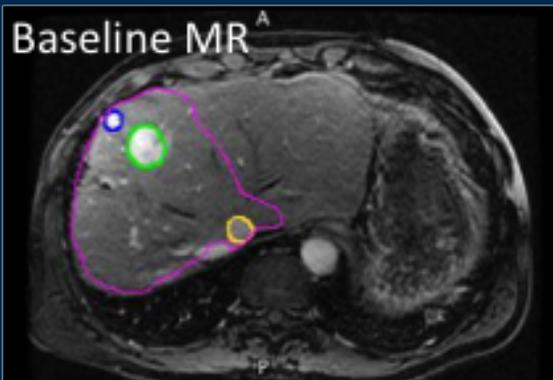


Gnesin et al, JNM 2016

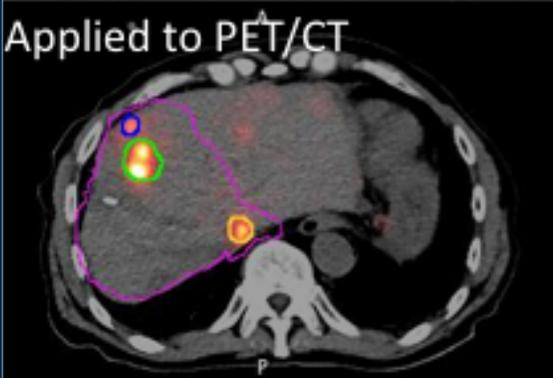


Haste et al, J Vasc Interv Radiol 2017

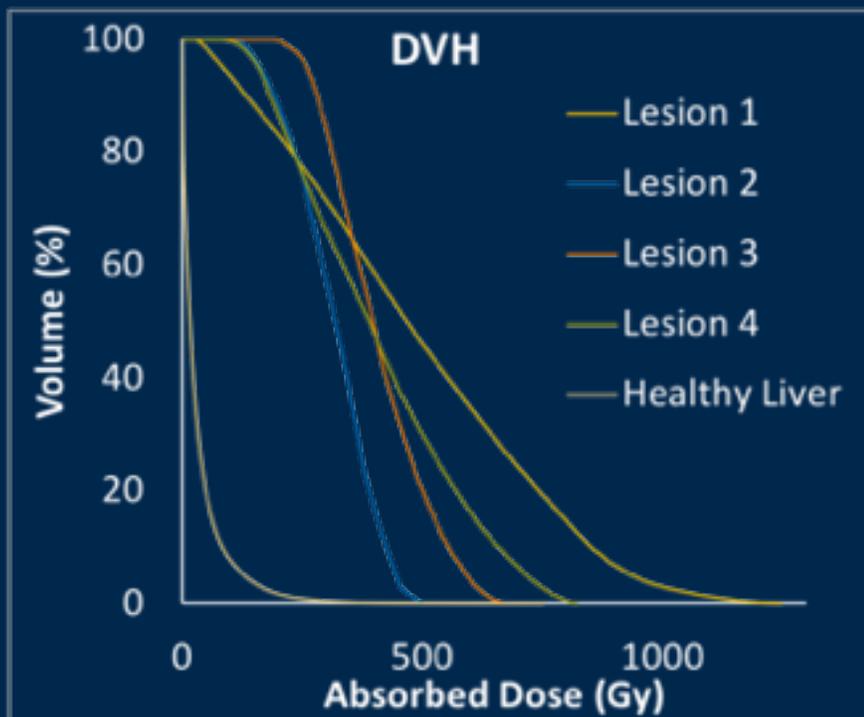
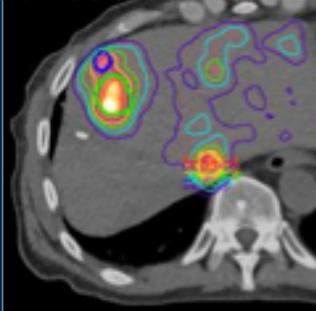
Patient example: Y-90 PET/CT based dosimetry



MR defined lesions

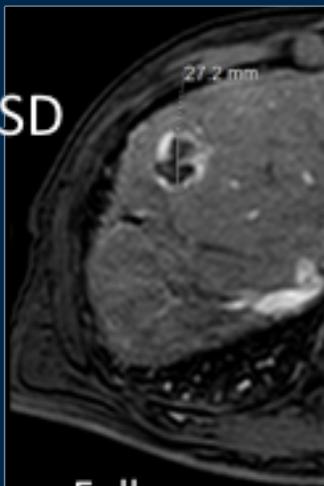


Isodose contours

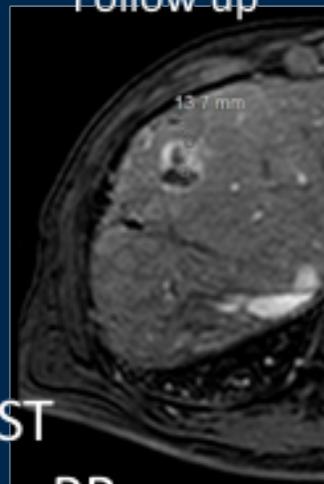
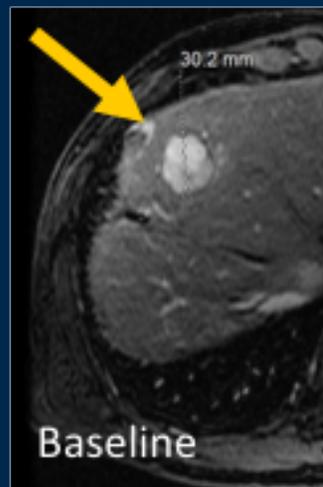


Name	Volume cc	Max Dose (Gy)	Min Dose (Gy)	Mean Dose (Gy)	SD
Lesion 1	11	1256	23	488	268
Lesion 2	1	504	99	313	85
Lesion 3	2	674	177	407	102
Lesion 4	5	825	69	404	175
Healthy Liver	1140	780	0	33	49

RECIST
Criteria: SD



Follow up



mRECIST
Criteria: PR

Lesion Dose-Response

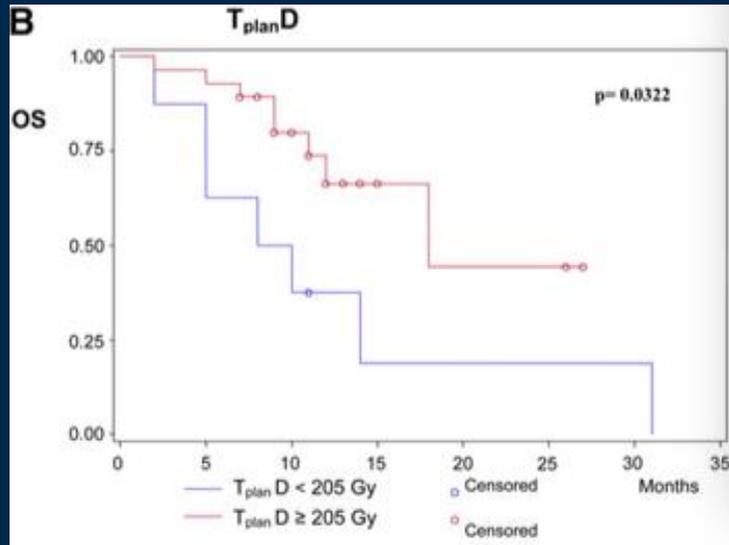


Absorbed dose significantly ($p < 0.05$) associated with shrinkage. Median absorbed dose among responding and non-responding tumors was **209** and **130 Gy** ($p=0.024$) with RECIST and **271** and **97 Gy** ($p=0.004$) with mRECIST criteria.

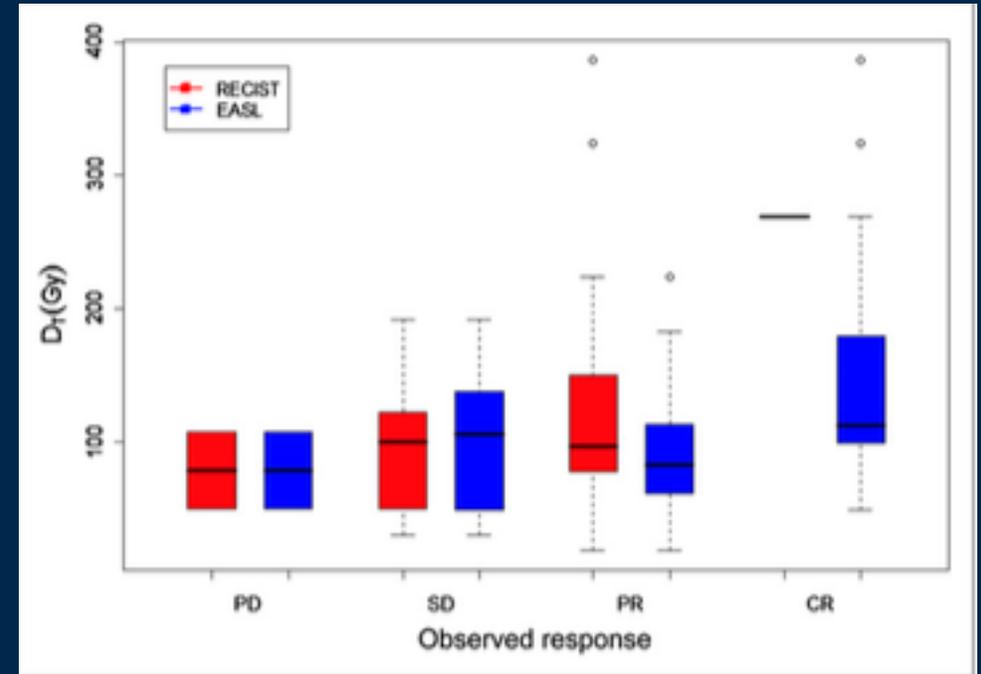
^{90}Y RE with glass microspheres: past dose-response studies

- Threshold lesion dose predictive of response around 100-500 Gy
- Mostly based on predicted doses from Tc-MAA SPECT/CT
 - Garin, JNM 2012 (predictive of survival in HCC); Chiesa, EJNM 2015 (predictive of response in HCC); Kokabi, J Vasc Interv Radiol, 2014 (predictive of survival in HCC)
- Post therapy imaging based
 - Y-90 Bremsstrahlung SPECT/CT based
 - Strigari et al, JNM 2010 (predictive of response in HCC)
 - Y-90 PET/CT based
 - Fowler et al, Cardiovasc Interv Radiol, 2016 (dose-response for CRC only); Srinivas et al, Front in Oncol, 2014 (HCC no dose- response)

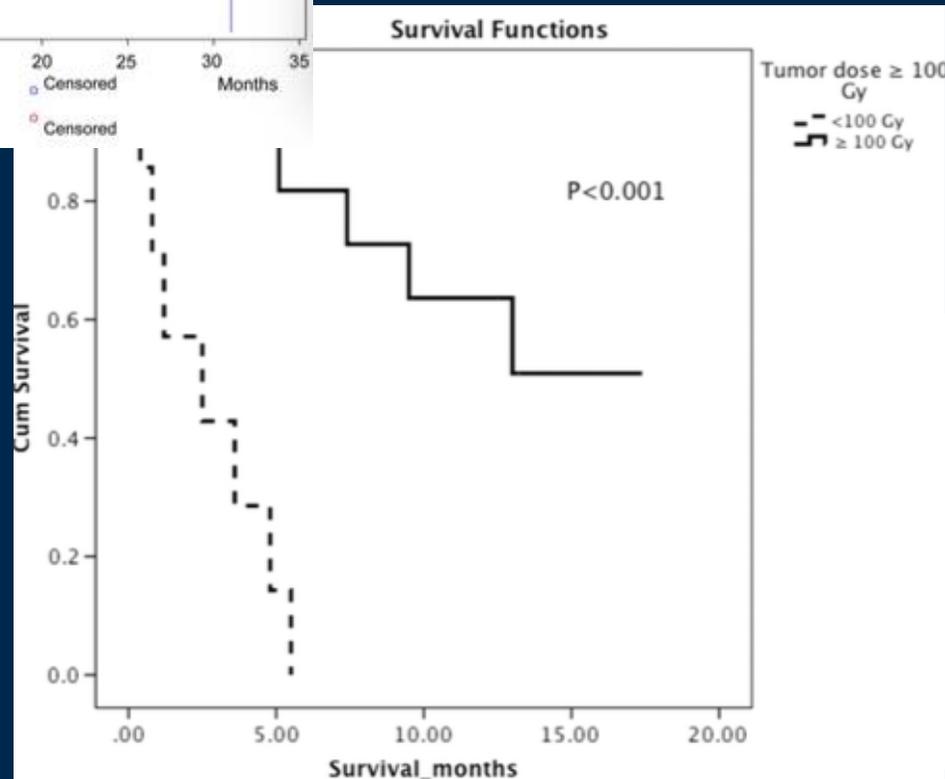
Y-RE: Past dose - response studies



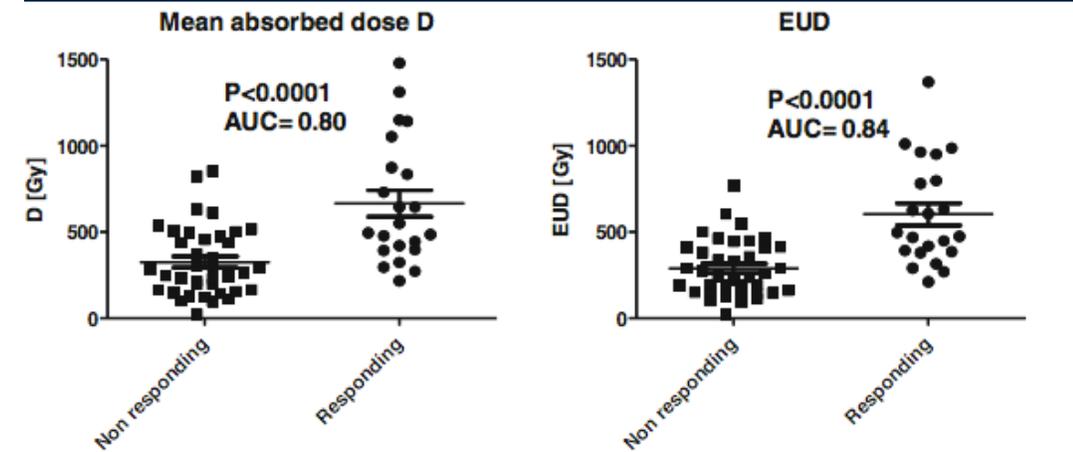
Strigari et al



Garin et al



Kokabi et al



Chiesa et al

Thank You

To patients who volunteered for the presented clinical studies.

To collaborators Jeff Fessler PhD, Pete Roberson PhD, Scott Wilderman PhD, Kyle Cuneo MD, Bill Majdalany MD, Dawn Owen, MD, Ravi Kaza MD, Ravi Srinivasa MD, Justin Mikell PhD

Funding from NIH(NIBIB) grant R01EB022075 is Acknowledged

yuni@umich.edu

